

# MR Imaging of MASH

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UC San Diego



# Disclosures

- Grant support-Bayer, Pfizer, Siemens, GE, Median
- Consulting-Bayer, epigenomics, GE

**MASLD**

**MASH**

- **Ethnicity**
- **Obesity**
- **DNA**
- **T2DM**
- **Met Sx**

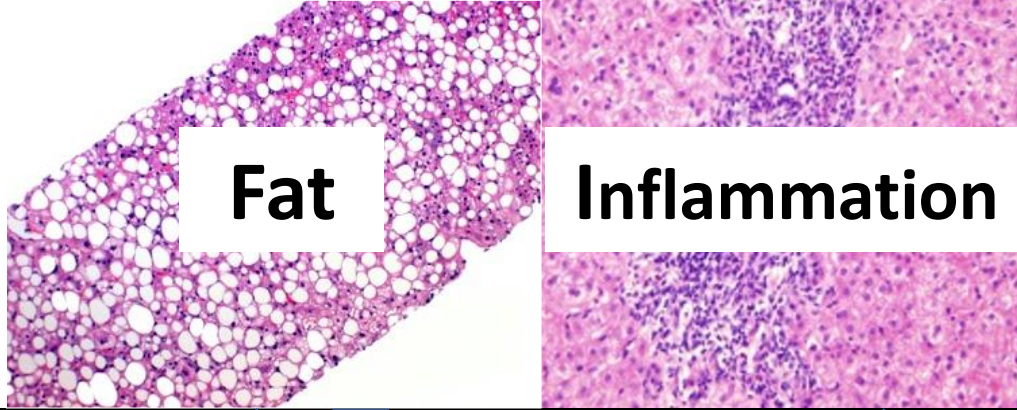


**Lipogenesis**

**MALSD**

**MASH**

- Ethnicity
- Obesity
- DNA
- T2DM
- Met Sx



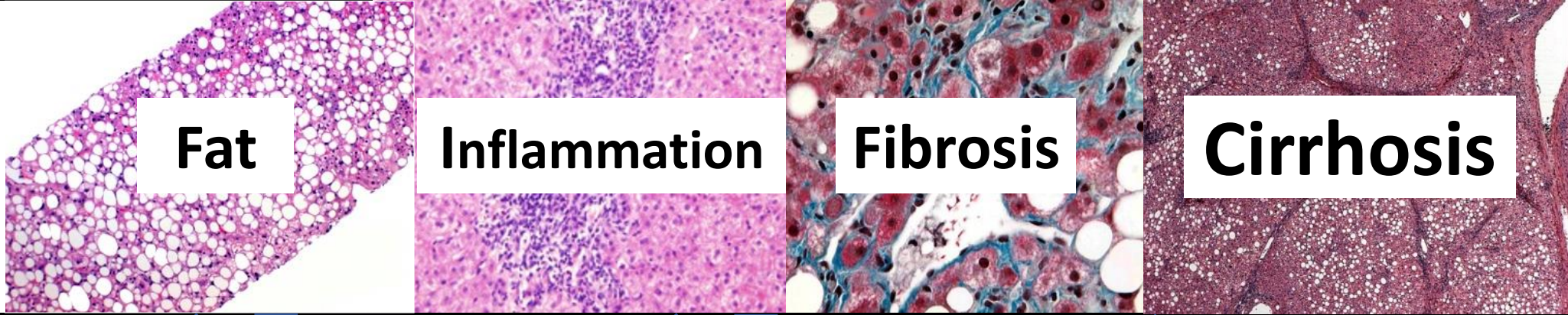
Lipogenesis

Oxidative stress  
Apoptosis  
Cytokine activation

**MASLD**

**MASH**

- Ethnicity
- Obesity
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- T2DM
- Met Sx



Lipogenesis

Oxidative stress  
Apoptosis  
Cytokine activation

Progressive damage  
Scarring

**MASLD**

**MASH**

**Cancer**

**GIB**

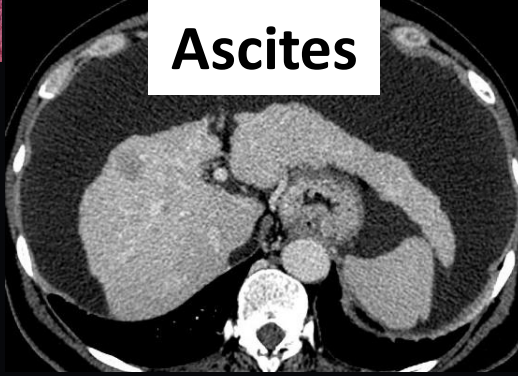
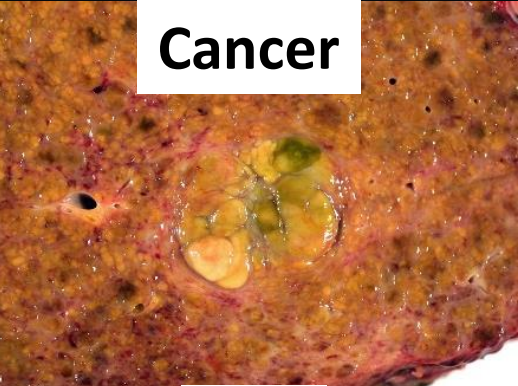
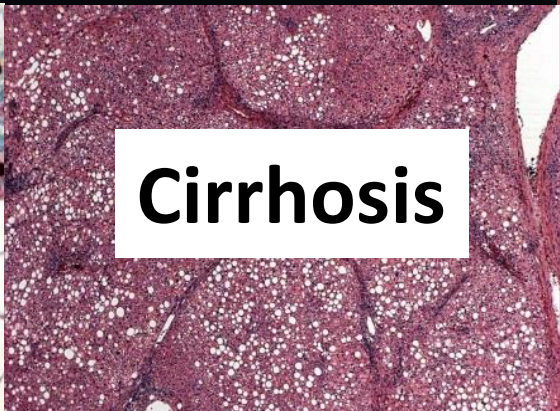
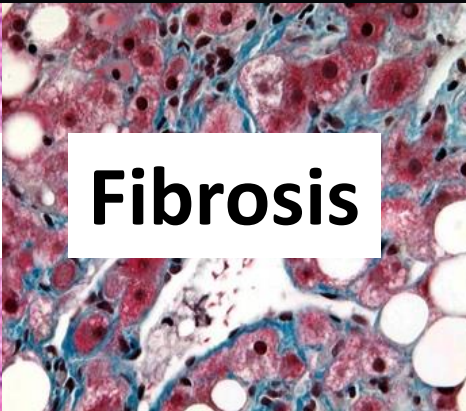
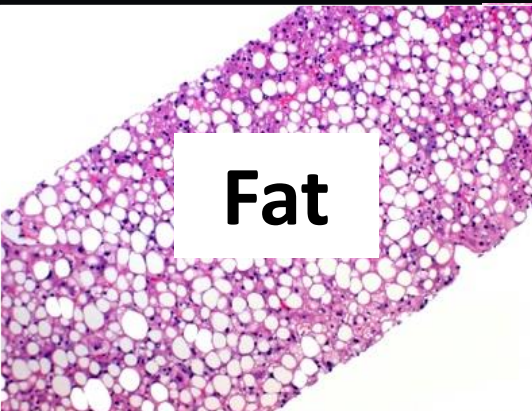
**Ascites**

**Fat**

**Inflammation**

**Fibrosis**

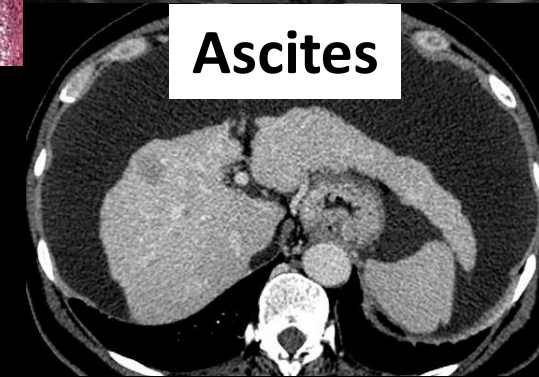
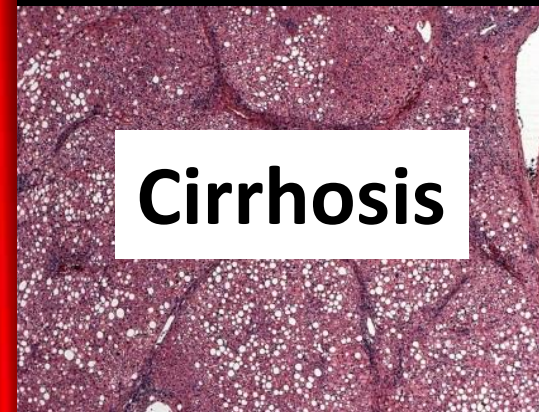
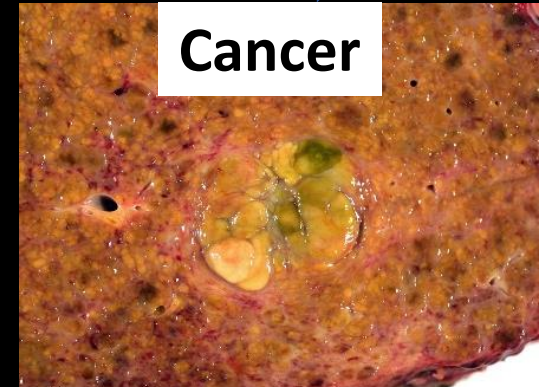
**Cirrhosis**



MASLD

MASH

Silent!





"horse left barn" Paul murphy @ Pinterest.com



Whats-thesayinganswers.com



**MASLD**

**MASH**

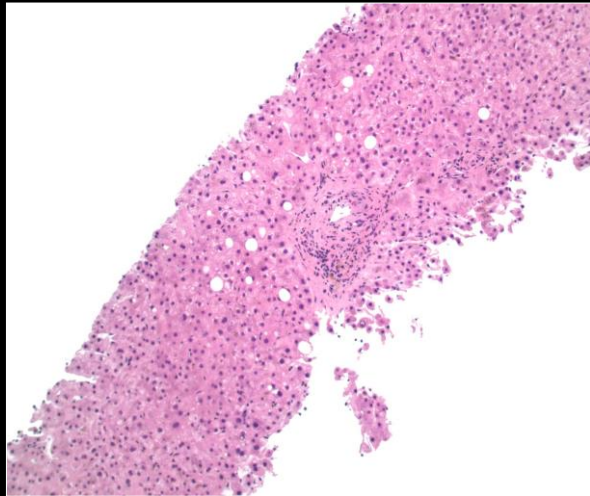
- **Ethnicity**
- **Obesity**
- **DNA**
- **T2DM**
- **Met Sx**



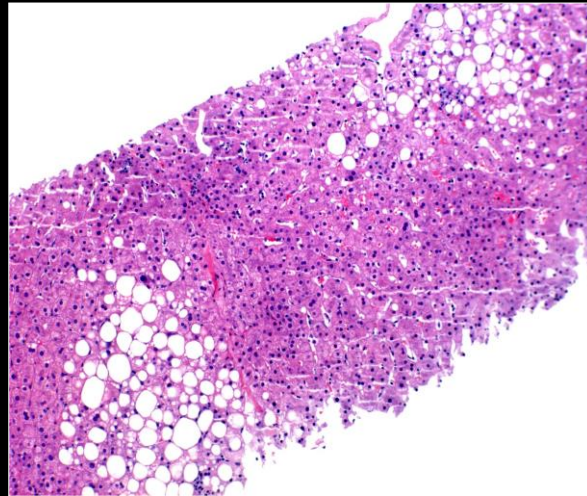
**Lipogenesis**

# Range of fat in liver

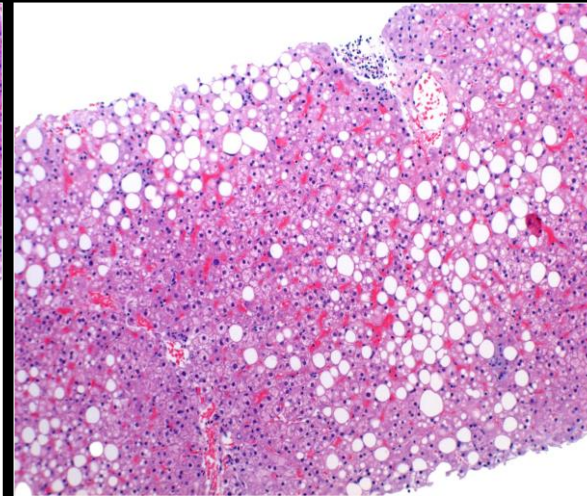
## Steatosis



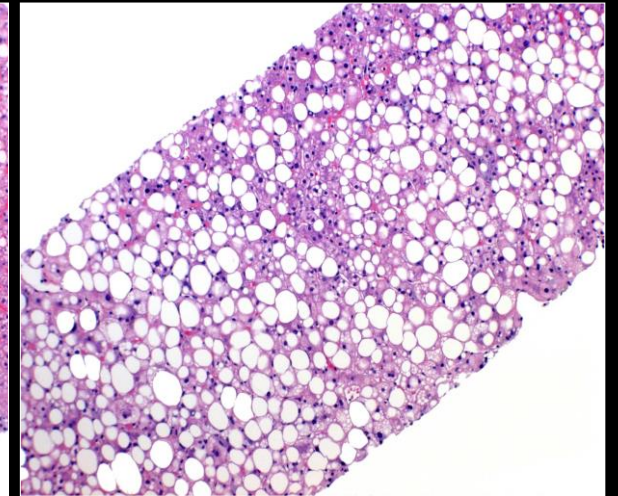
Minimal



Mild



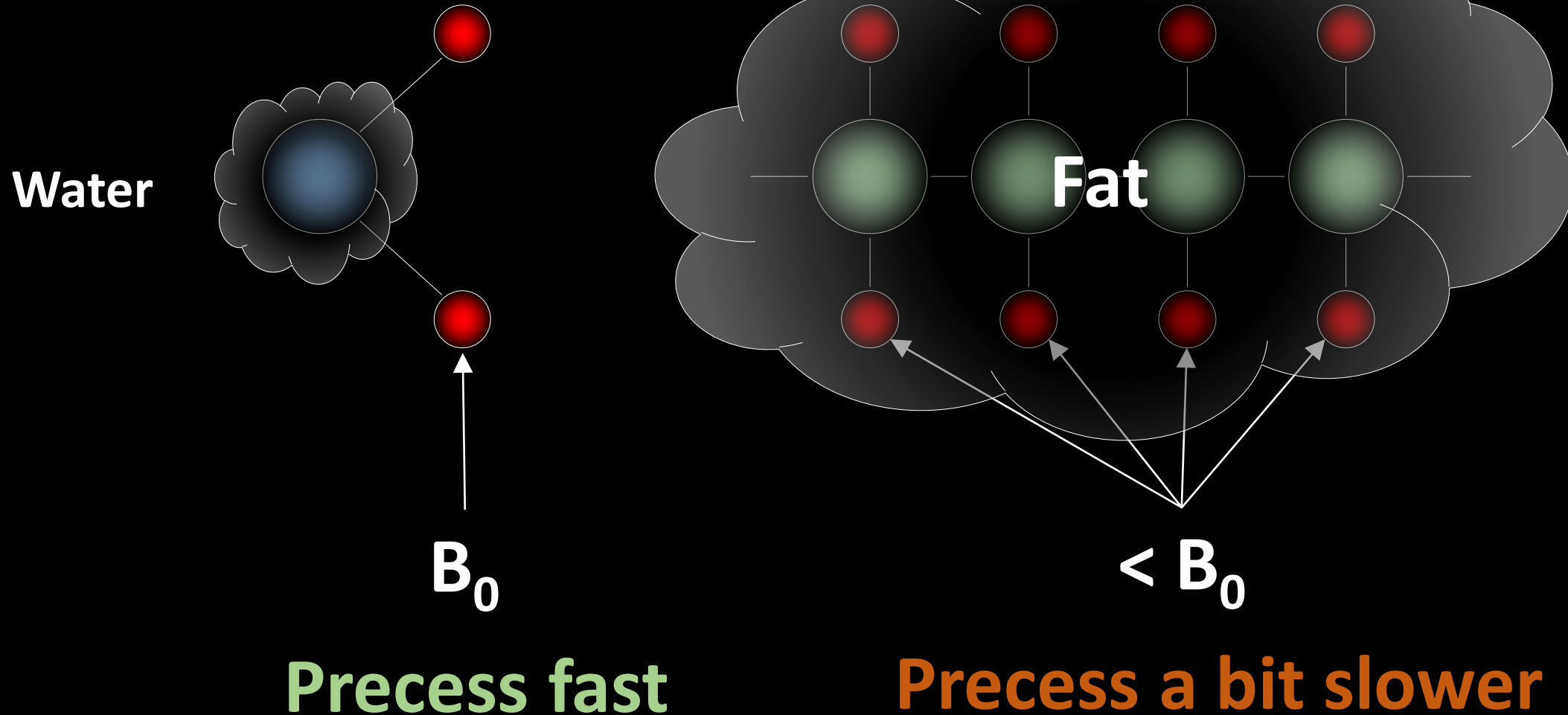
Moderate



Severe

How do we image Fat?

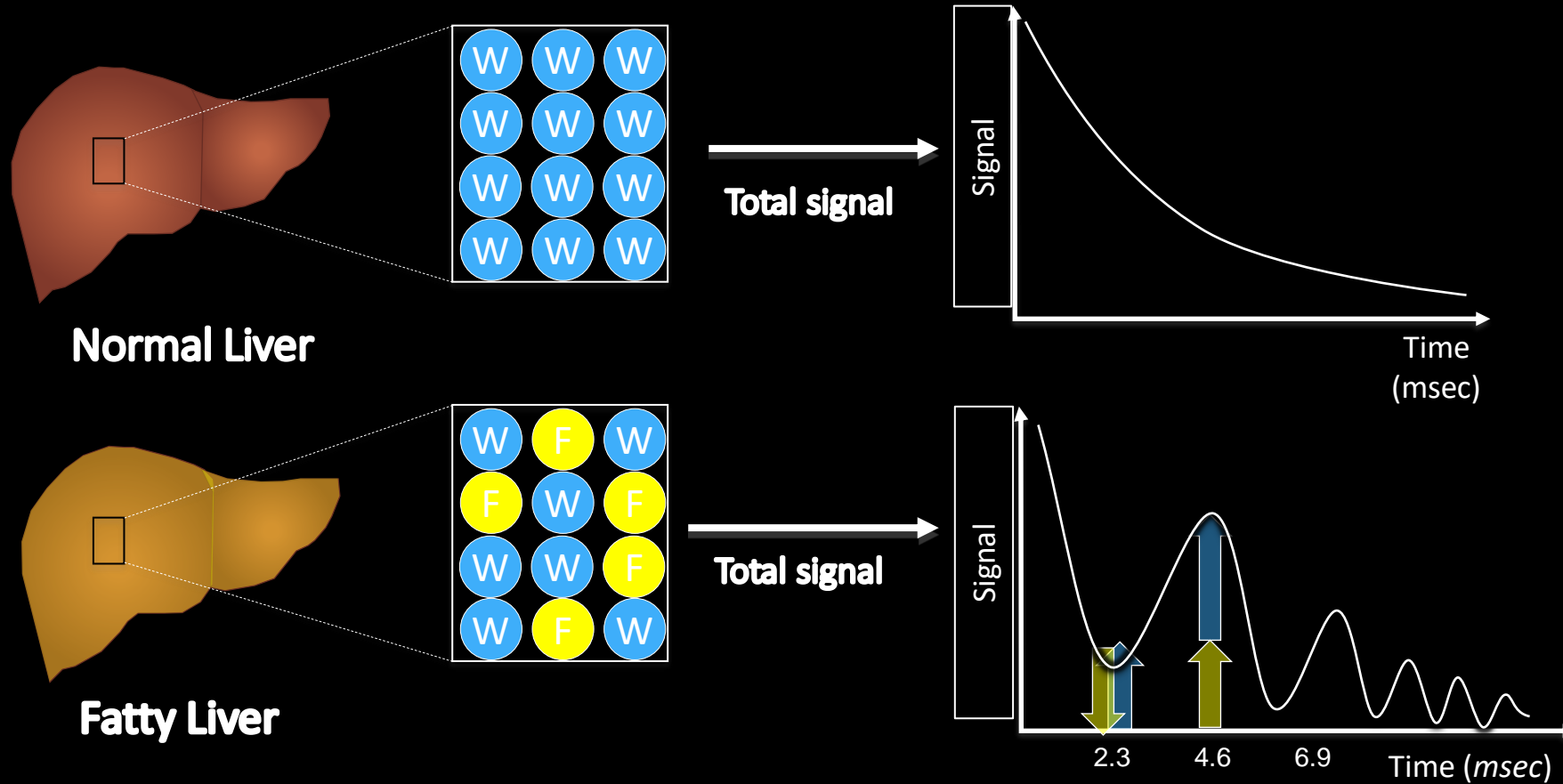
# Chemical Shift



Larmor Frequency differences

# Chemical Shift

at  $B_0 = 1.5T$

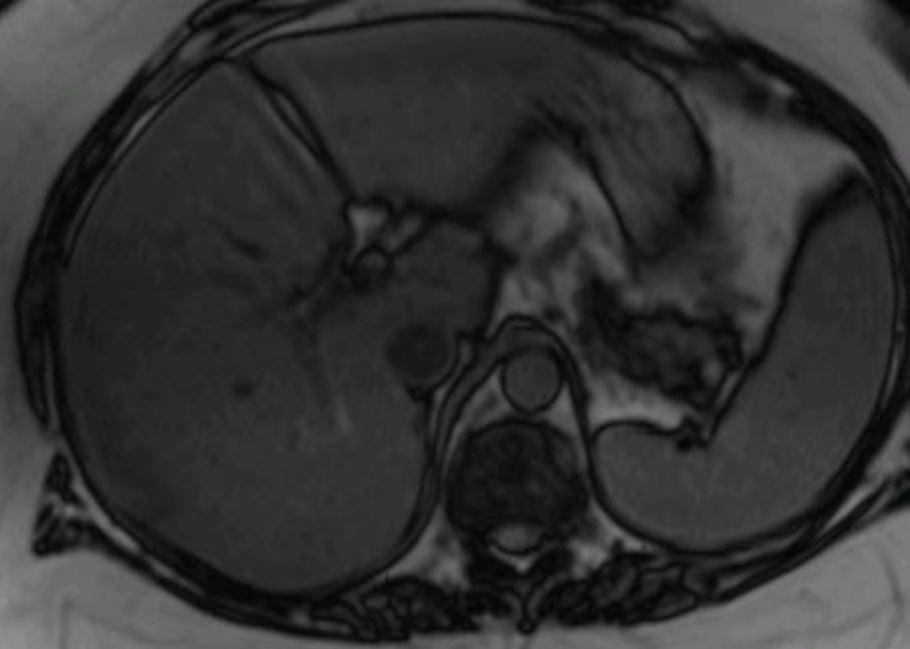
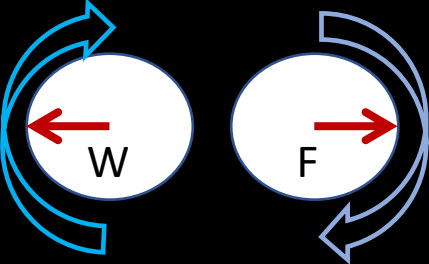


If Opposed  $\rightarrow$  [ Water - Fat ]

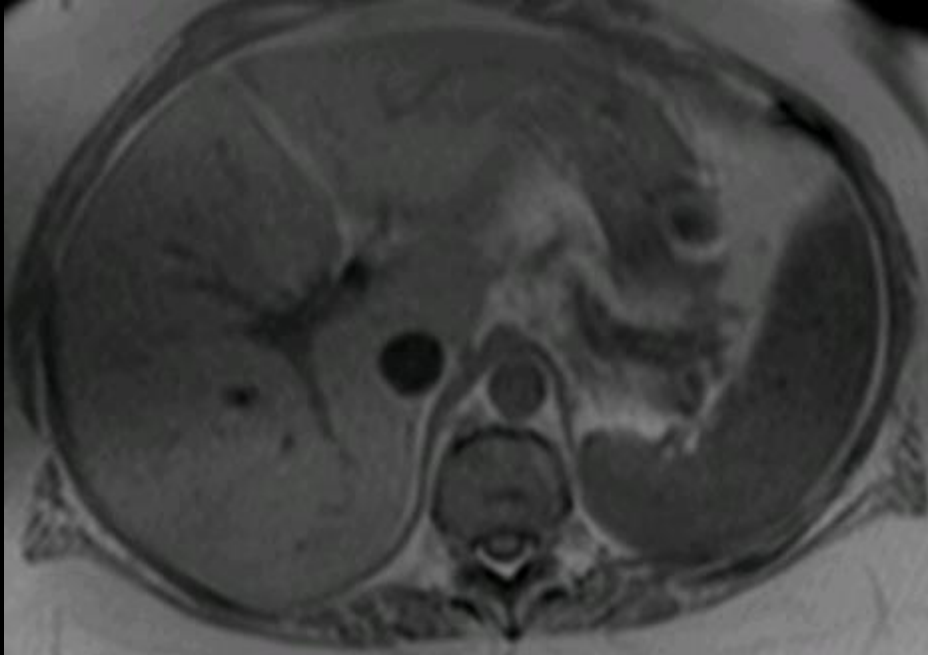
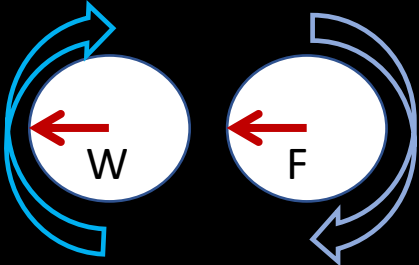
If In-phase  $\rightarrow$  [ Water + Fat ]

# Dual Echo MRI

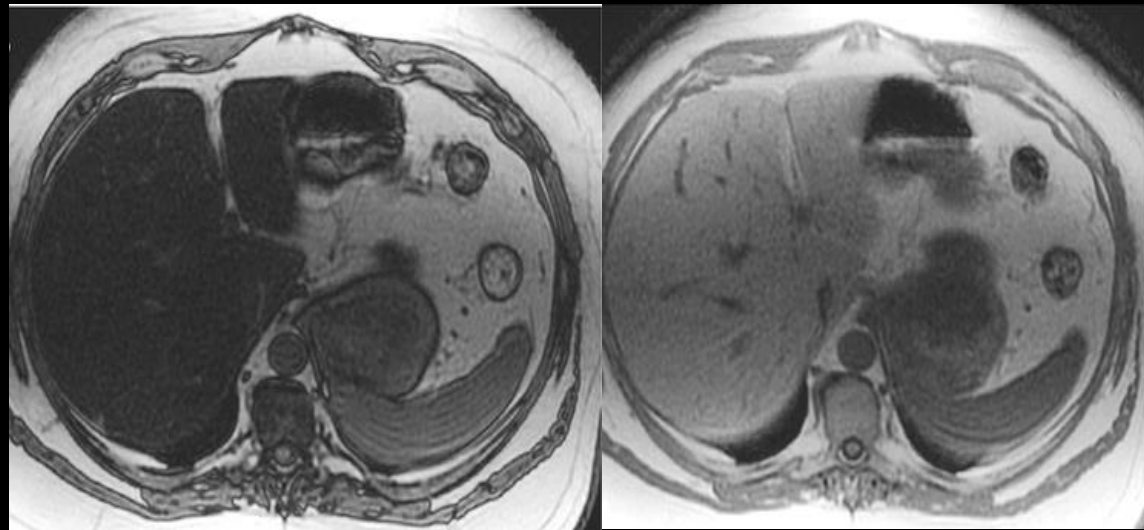
Out of phase



In phase



Loss of signal on out of phase due to fat



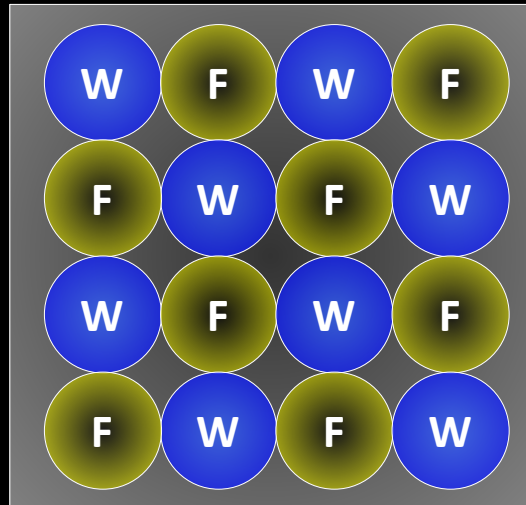
# Conventional dual echo MRI



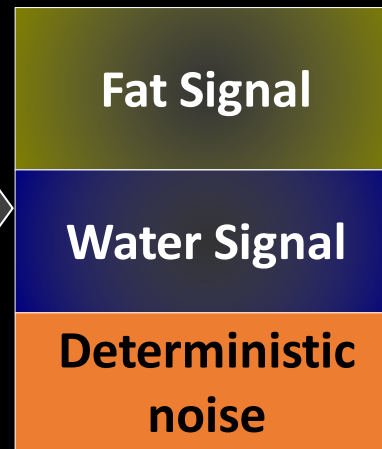
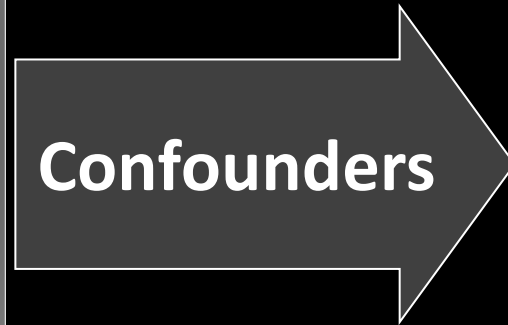
How much  
fat?



# Not good for Quantification



True Tissue  
Fat Content

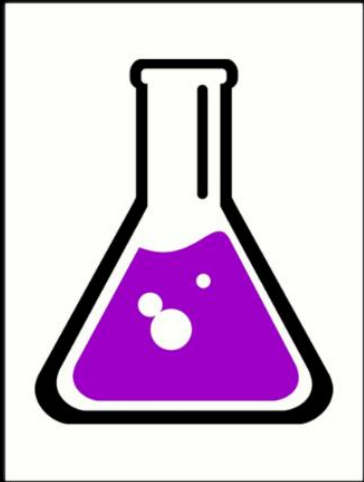


Signal  
Fat  
Fraction

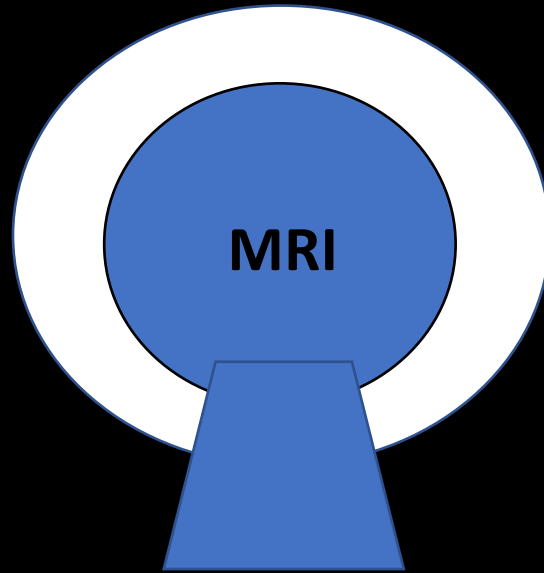
Results are  
not pure  
impacted by  
confounders

# How to Quantify

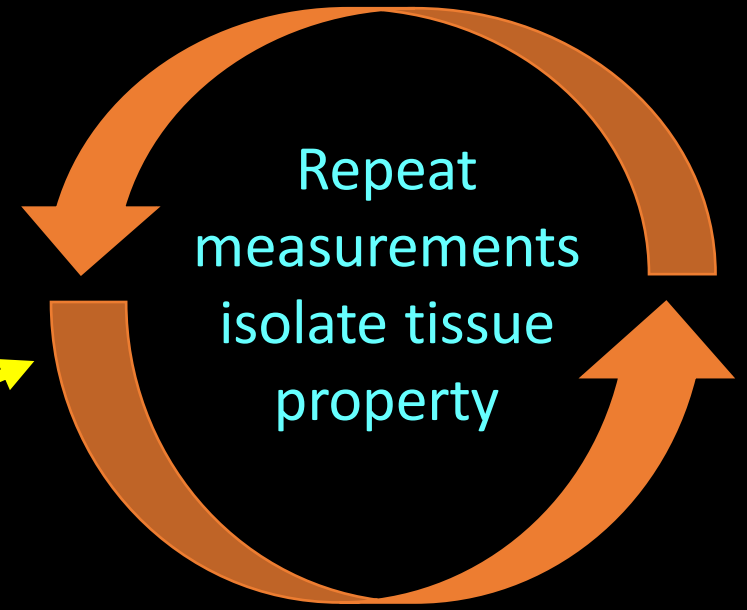
- MRI=signal intensity



Unknown parameter  
-tissue property  
-confounders



Known  
parameters  
(adjust TE)

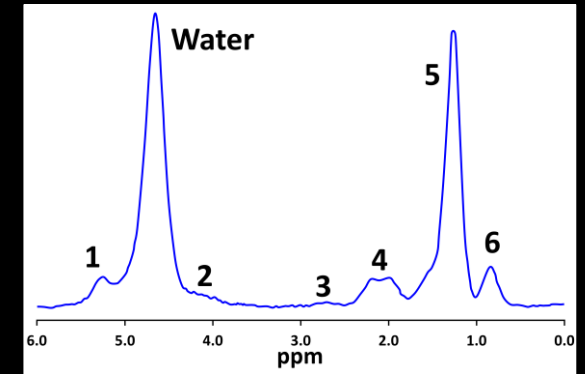


Quantitative data=  
deterministic noise  
+ tissue property

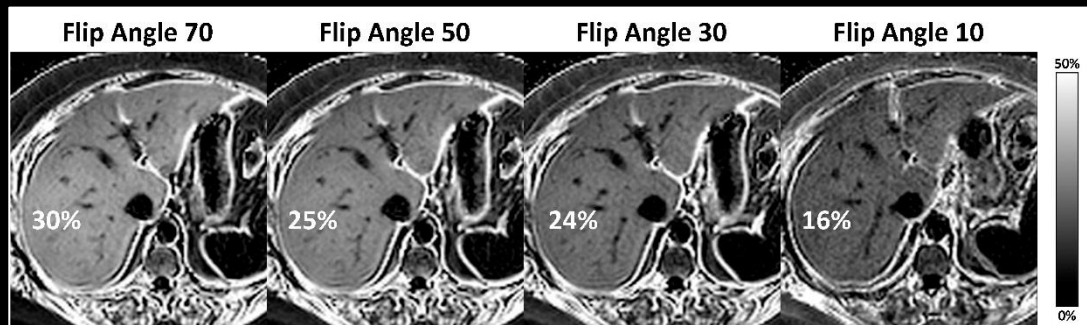
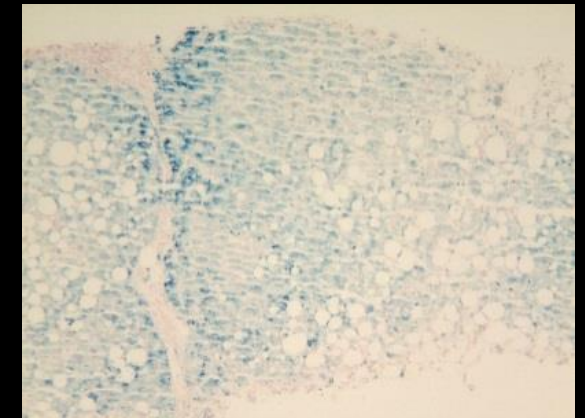
# Confounders

- Complicated interference pattern,  
Different fat protons experience different magnetic fields

The solution: incorporate a typical fat spectrum



T<sub>1</sub> bias—fat has shorter T1 than water, T1-weighting amplifies fat signal

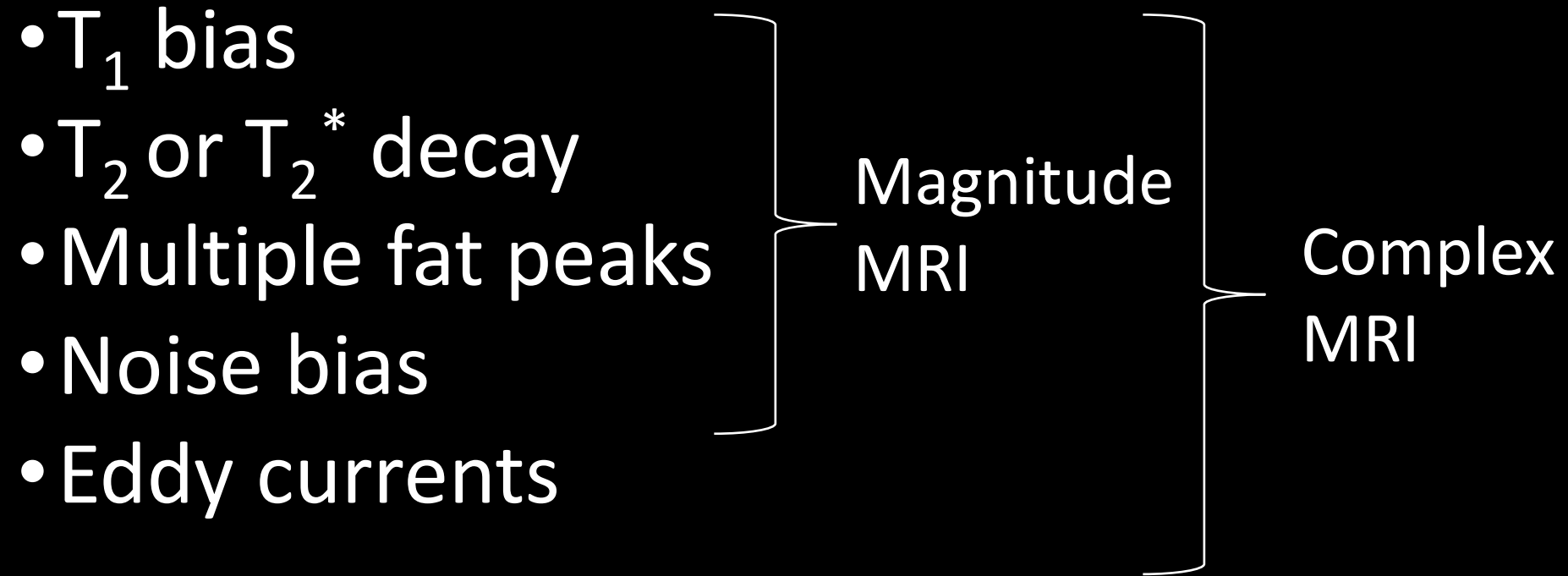


Solution: minimize T<sub>1</sub> bias via low FA or long TR

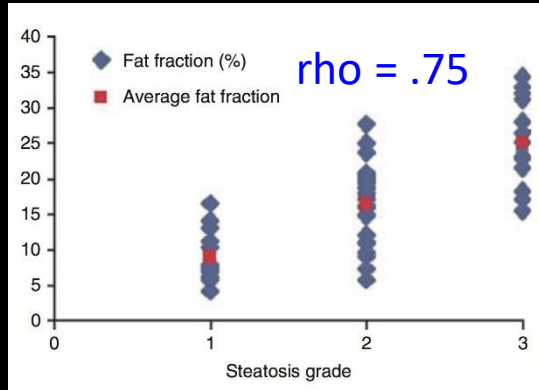
Iron causes T<sub>2</sub><sup>\*</sup> decay

Solution: correct for decay by acquiring multiple echoes

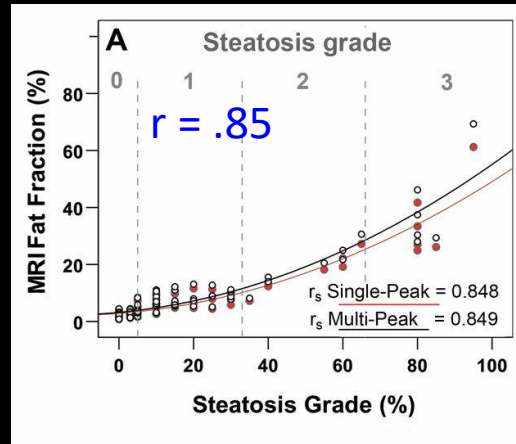
# MRI-PDFFF --- Quantitative Imaging Biomarker



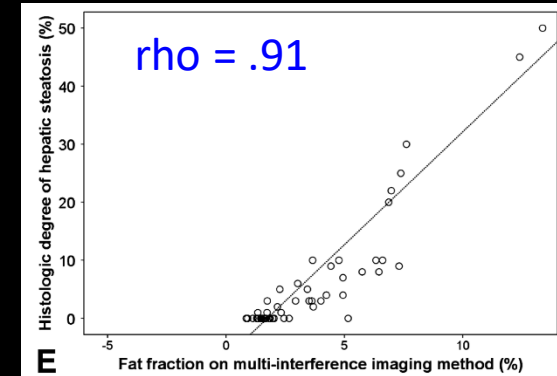
# MRI-PDFF --- Correlates well with Histology



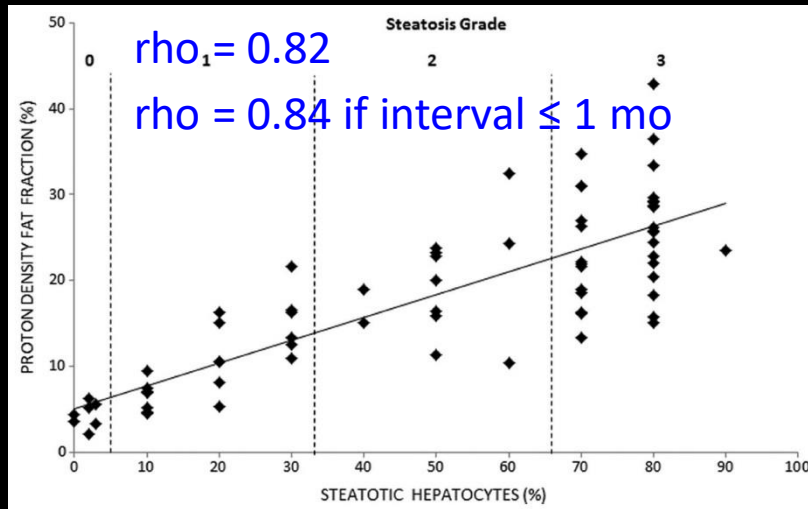
Permutt AP&T 2012  
(NAFLD)



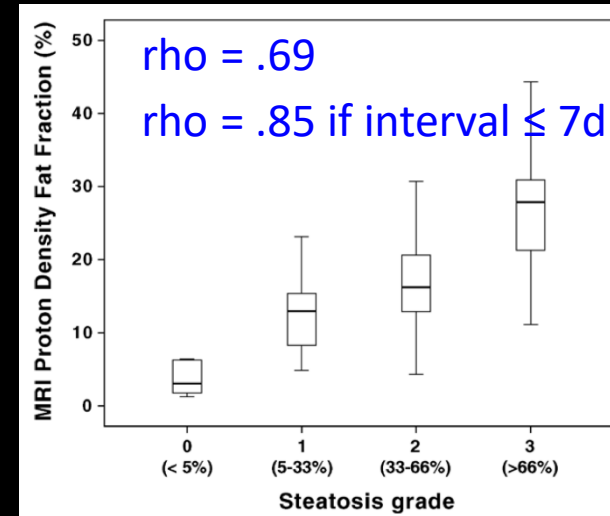
Kuhn et al Radiology 2012  
(Mixed Liver Disease)



Kang et al Invest Radiology 2012  
(Mixed Liver Disease)

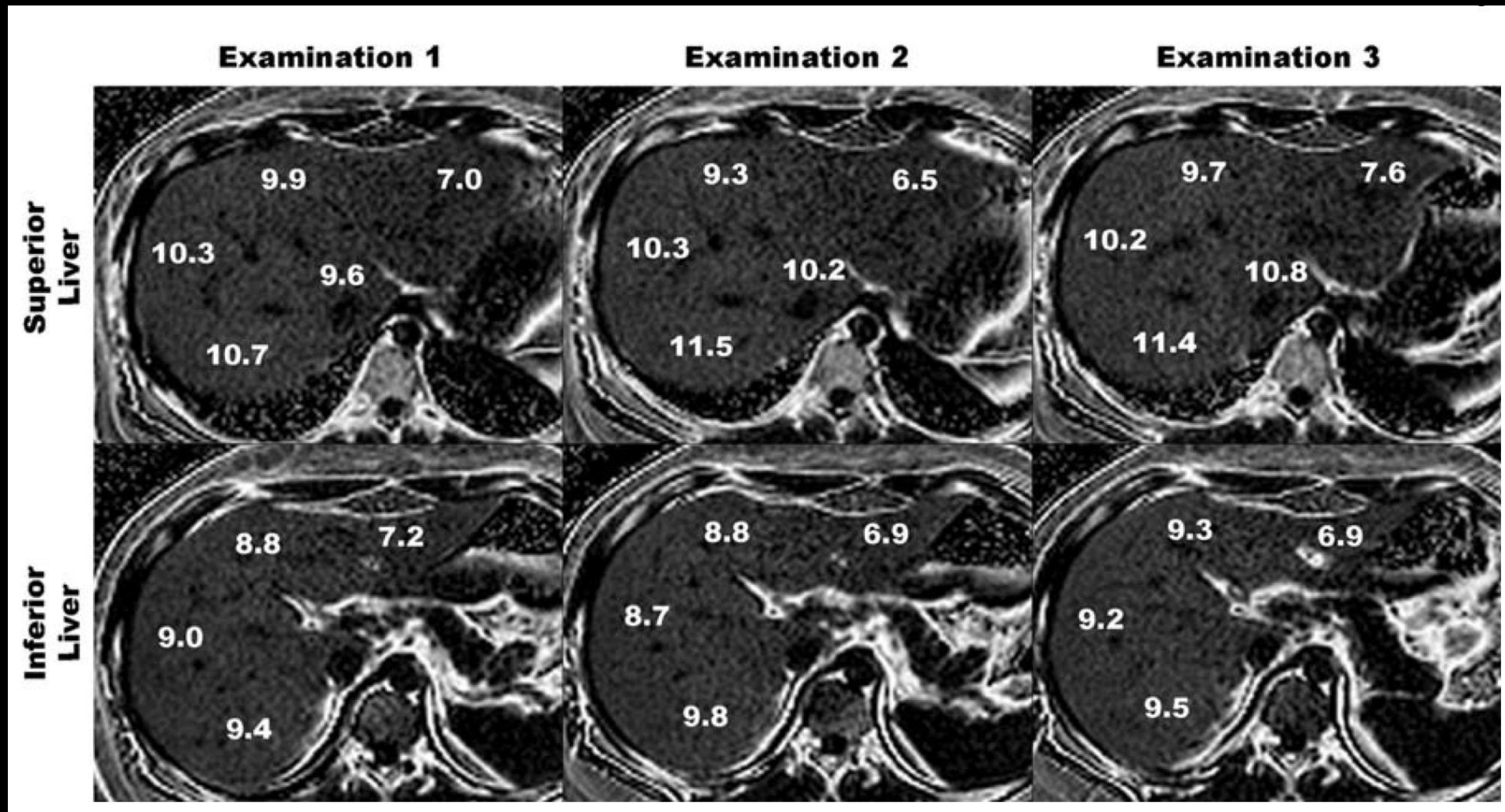


Idilman et al Radiology 2013  
(NAFLD)



Tang et al Radiology 2013  
(NAFLD: children & adults)

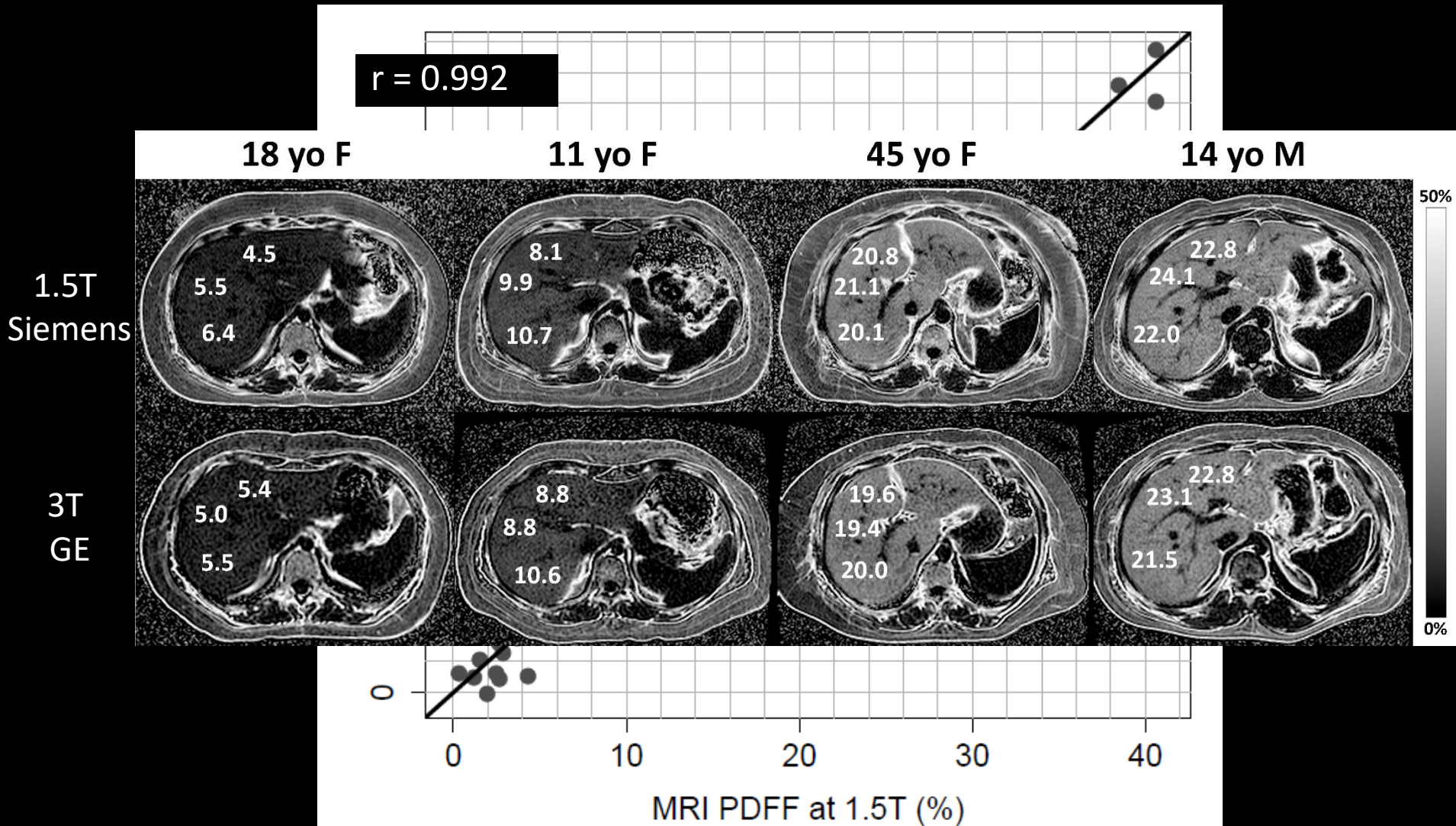
# MRI-PDFF --- Repeatable



Negrette et al. JMRI 2013  
Children & Adults with NAFLD

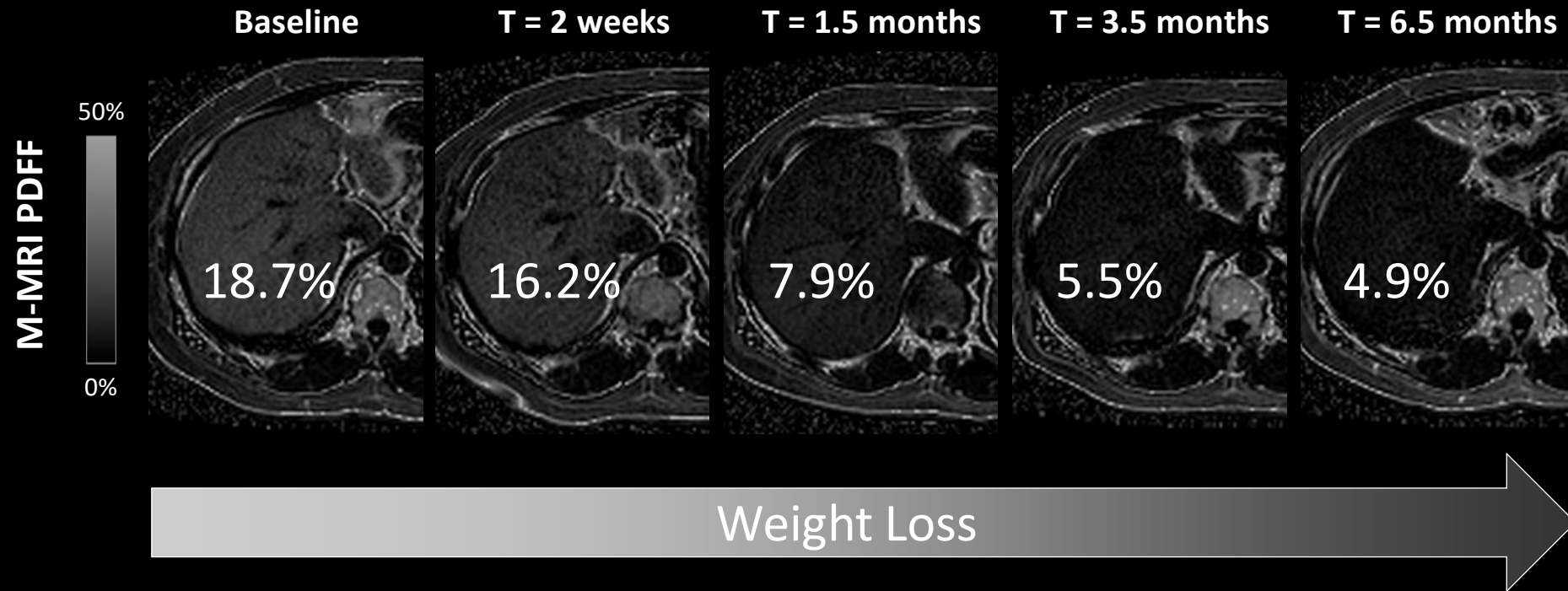
**SD of repeated examinations = 0.24 to 0.62 % points**  
**ICC of repeated examinations = 0.992 to 0.999**

# MRI-PDFF --- Reproducible across field strength



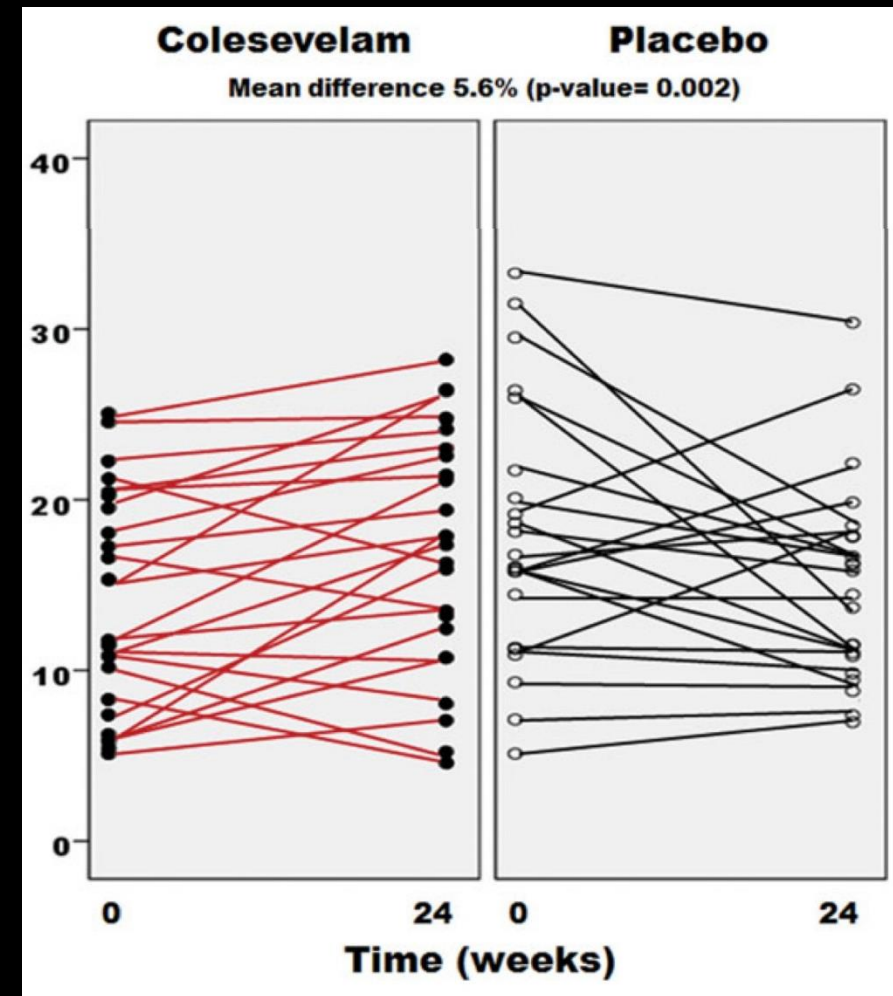
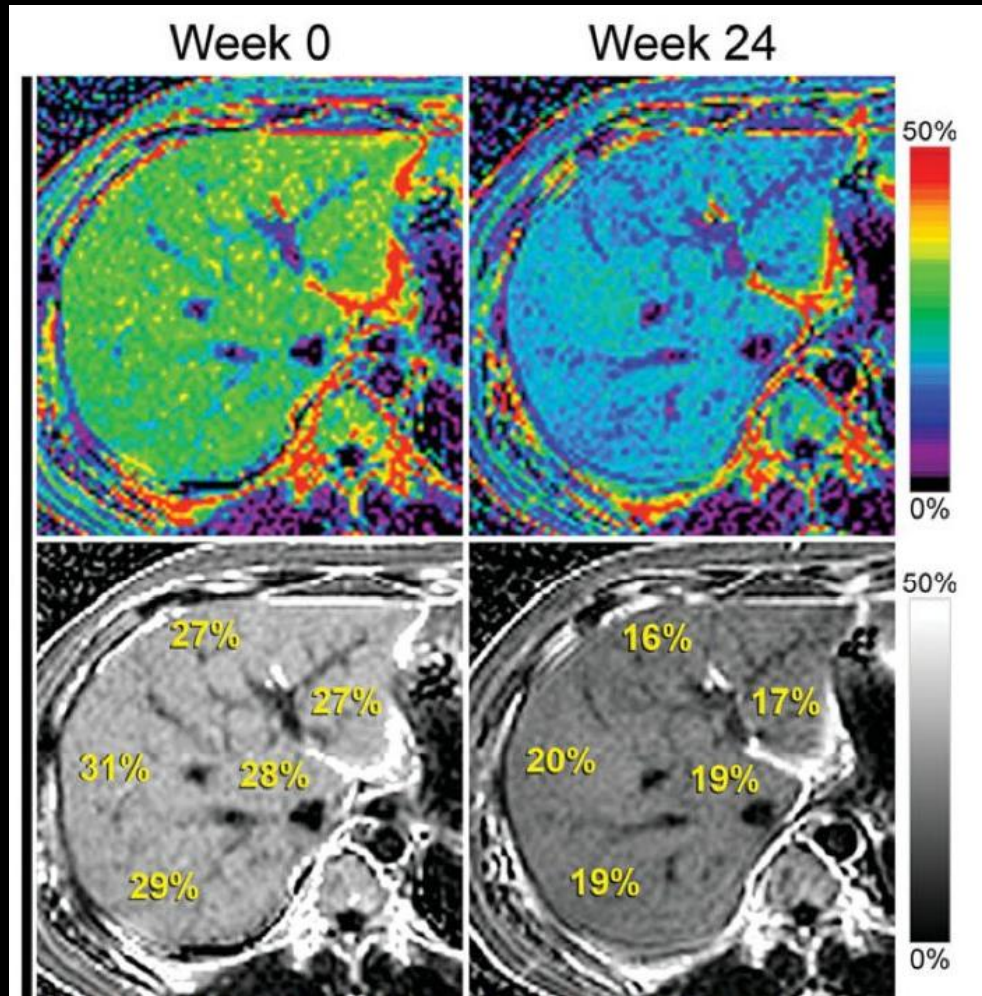
# MRI-PDFF accurately quantifies steatosis in NAFLD

## *Over Entire Range*

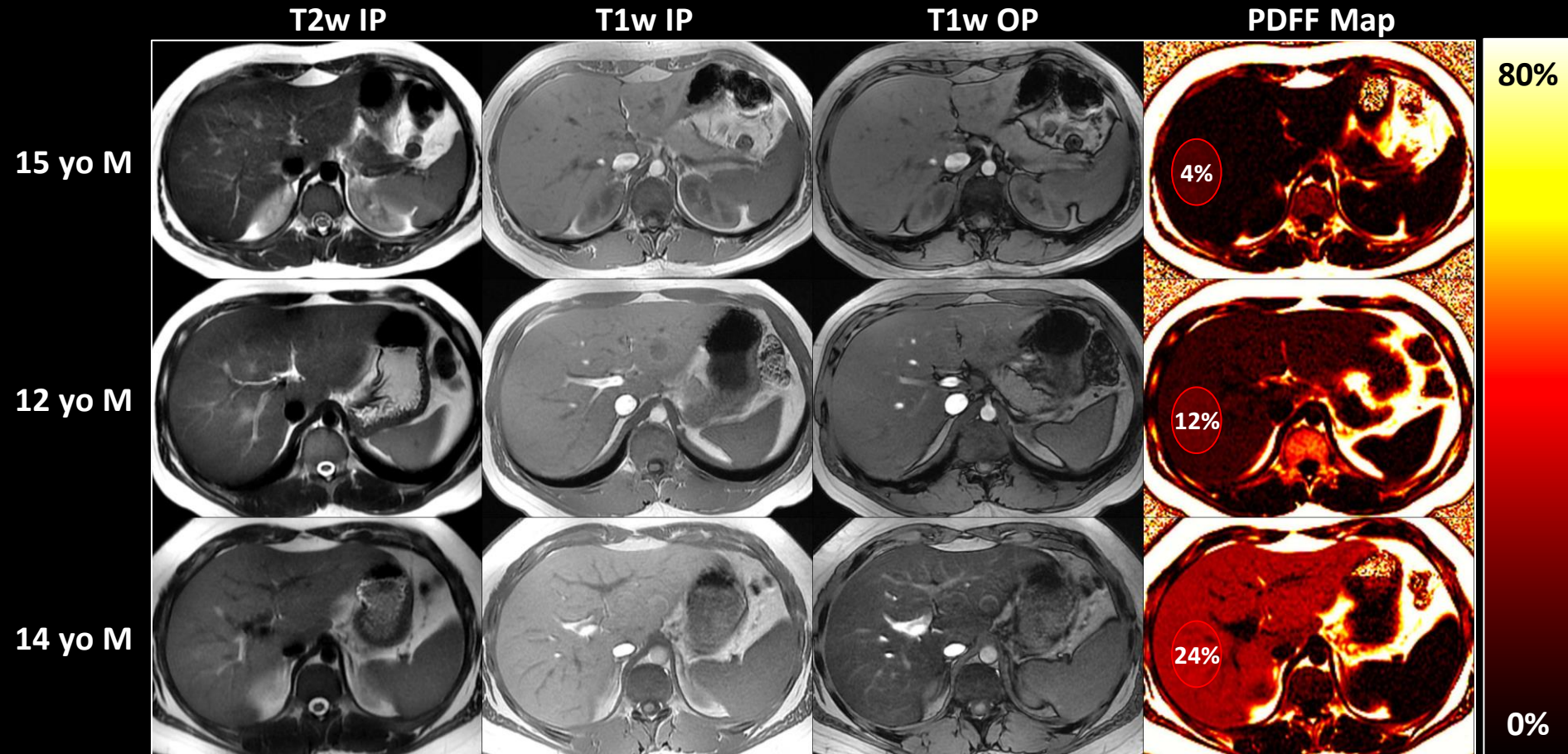




# MRI-PDFF --- Endpoint in Clinical Trials in NASH



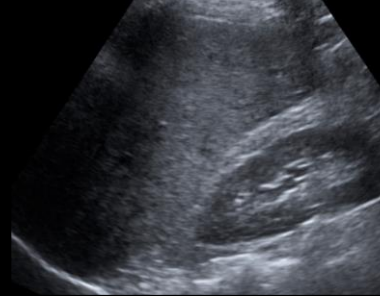
# Conventional MRI vs MRI-PDFF



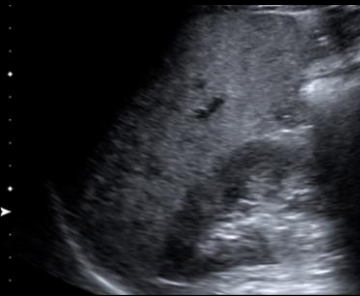
# Standard Ultrasound

Hepatorenal  
Index

Steatosis Grade 1



Steatosis Grade 2



Steatosis Grade 3



**Modest performance**

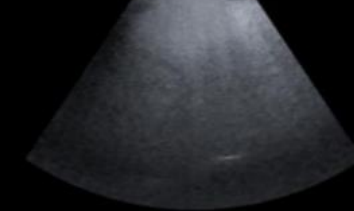
50-62% sensitive for steatosis > 5%



No blurring  
(15/16)



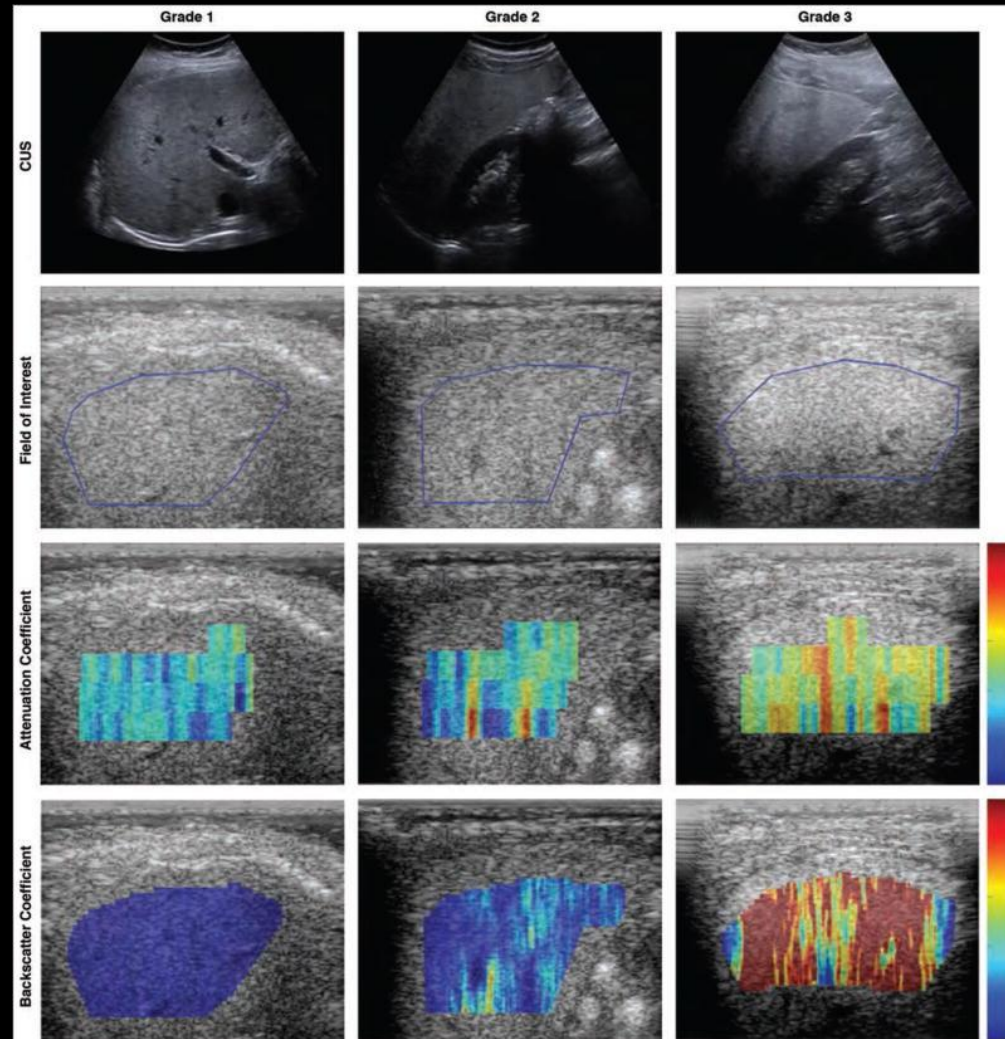
Mild-moderate blurring  
(14/16)



Severe blurring  
(15/16)

# Quantitative US

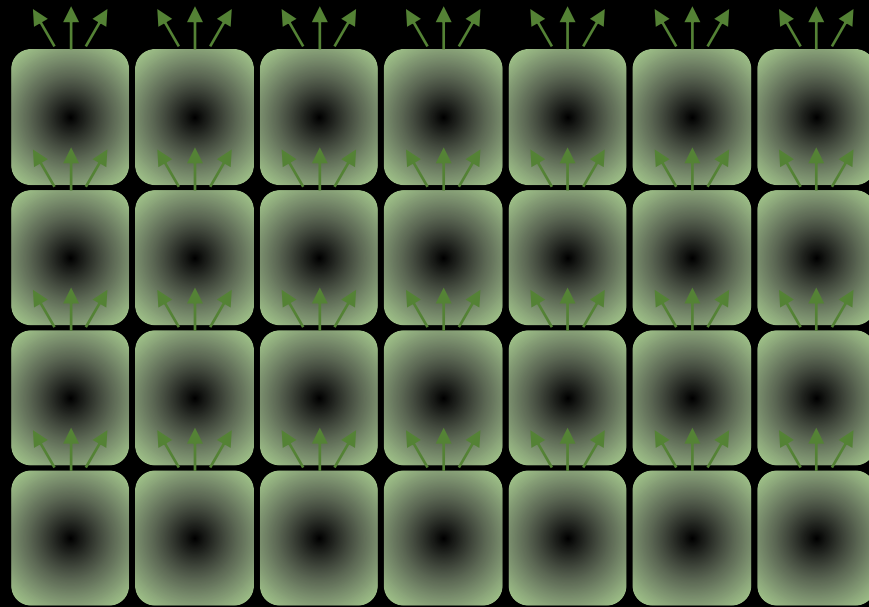
- Attenuation coefficient
  - -energy loss in tissue
- Backscatter coefficient
  - -sound waves returning
- Speed of sound
- 



# Concept: Fat droplets scatter and attenuate the ultrasound beam

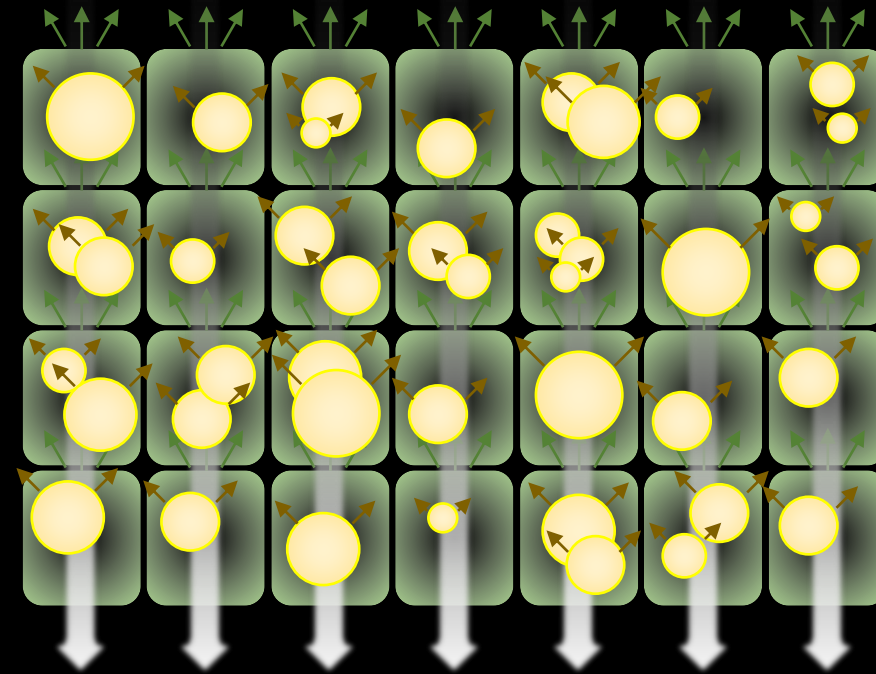
**Normal liver**

(some scattering by hepatocytes and other structures)



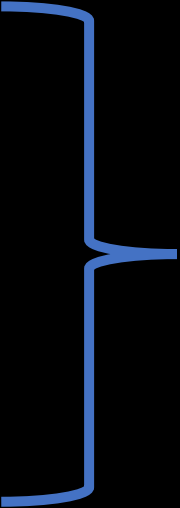
**Fatty liver**

(fat droplets act as additional scatterers)



# Attenuation Imaging on US systems

- ATI- Aplio i-series Canon
- ATT-Hitachi
- UGAP-GE systems
- UDFF-Siemens systems
- ATT Plus-Hologic
- TAI-Samsung Medison

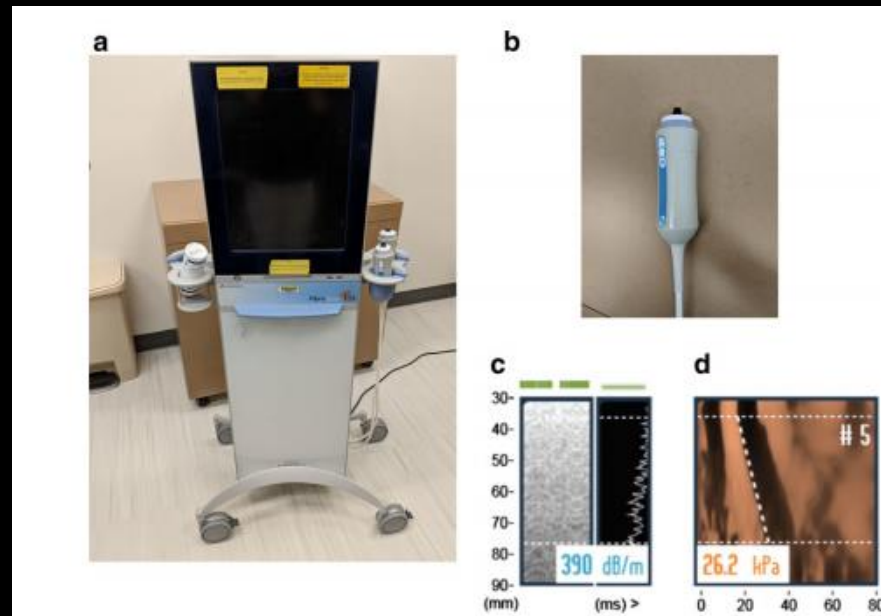


Values above 0.5-1.1  
dB/cm/MHz are abnormal

**Potential confounders:** fibrosis, etiology, fasting state, distribution of fat, technical parameters

# Controlled Attenuation Coefficient (CAP)

- Measured on VCTE machine-since 2010
- Variable thresholds reported
- AUC 0.82 for  $S > 0$ , 0.75 for  $S > 1$
- Confounders: CLD etiology, diabetes, BMI, AST, gender



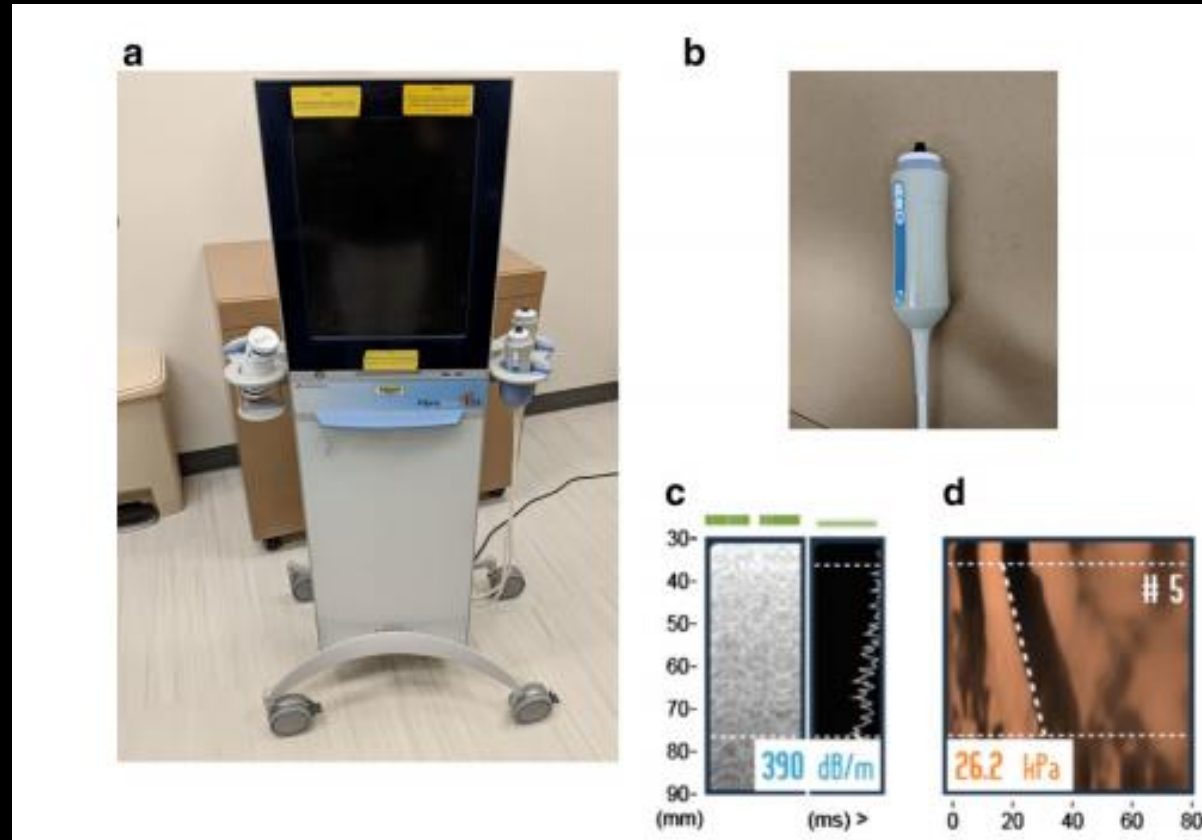
What is on the horizon?



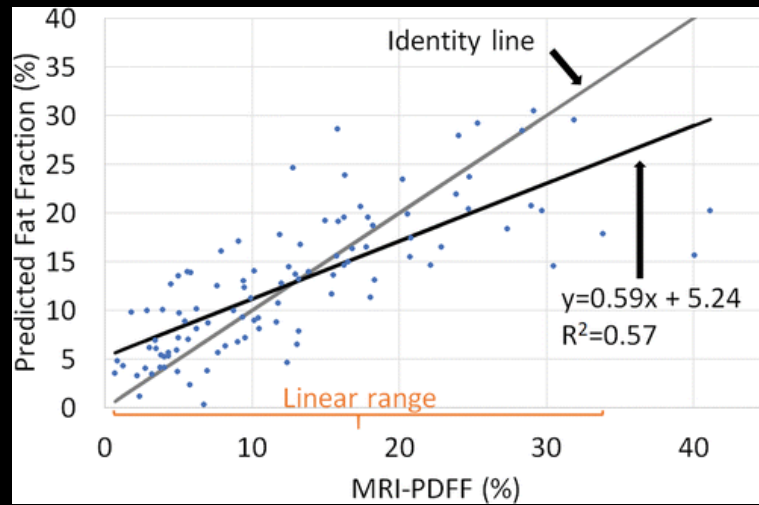
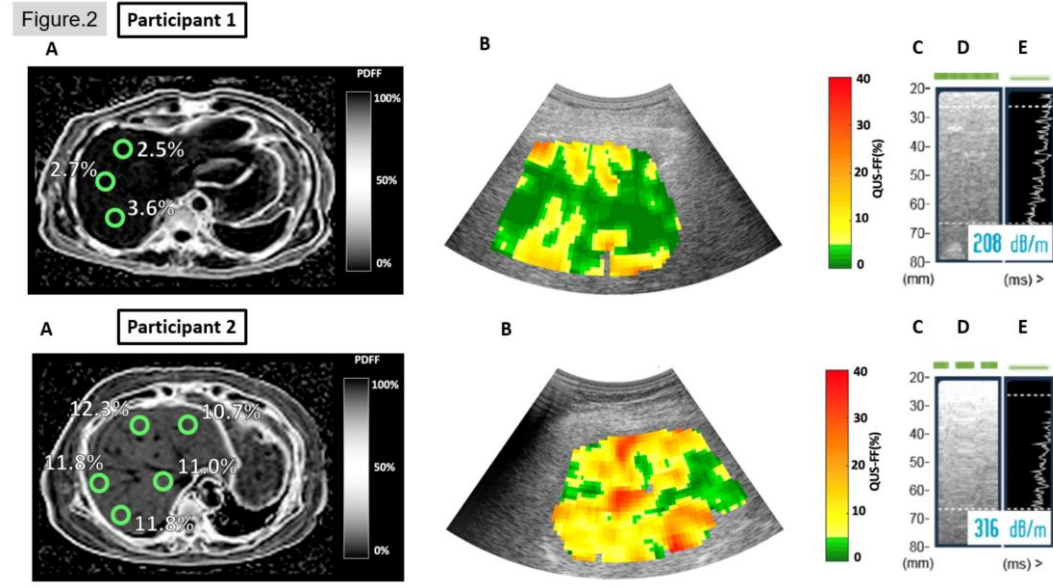


# Improved CAP

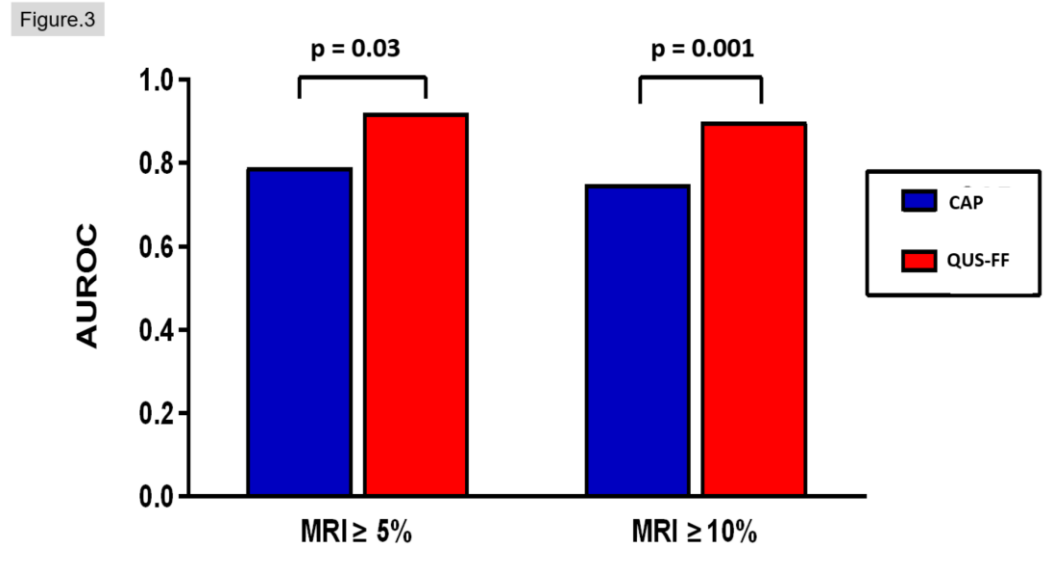
- New “Smart Exam” released in 2020



# QUS FF

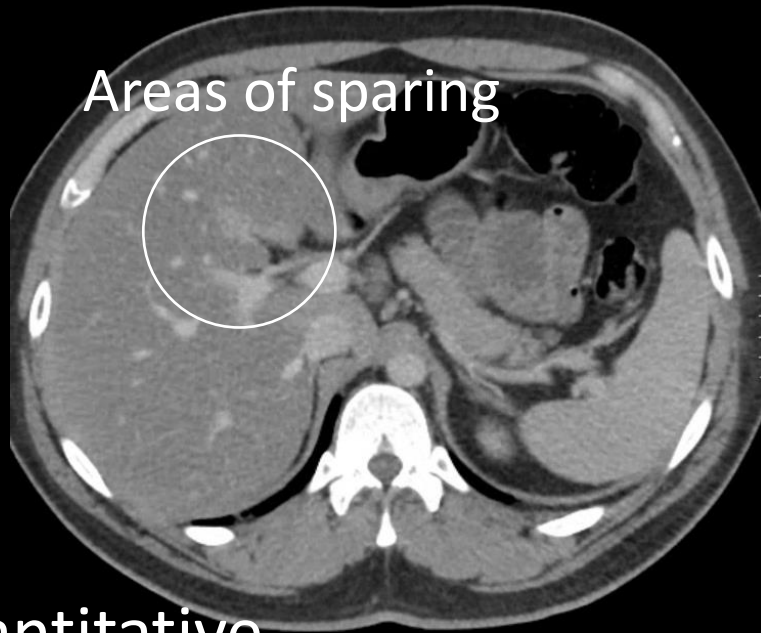


Han, Radiology 2020



Sirlin et al, unpublished data

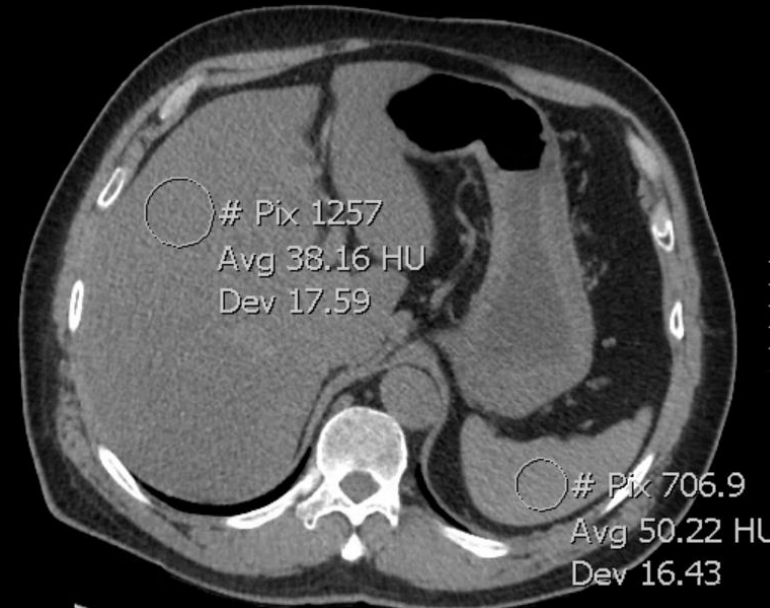
# Identifying Fat on CT



CT not quantitative

Not accurate for mild steatosis

Dependent on tube voltage



Liver HU-Splenic HU

## Table 2 CT<sub>L-S</sub> cut-off values and their ability to diagnose hepatic steatosis in the development cohort

From: [CT indices for the diagnosis of hepatic steatosis using non-enhanced CT images: development and validation of diagnostic cut-off values in a large cohort with pathological reference standard](#)

Diagnostic settings	Subjects who underwent CT at 120 kVp (n = 2733)				Subjects who underwent CT at 100 kVp (n = 579)			
	CT <sub>L-S</sub> cut-off values*	Sensitivity	Specificity	Accuracy	CT <sub>L-S</sub> cut-off values*	Sensitivity	Specificity	Accuracy
Diagnosis of HS ≥ 5%								
With 95% specificity	1.3 (0.8, 2.1)	33.9% (403/1188)	95.0% (1469/1545)	69.0% (1872/2733)	3.7 (2.7, 4.2)	38.7% (97/251)	95.1% (312/328)	70.6% (409/579)
With 95% sensitivity	13.6 (12.9, 14.0)	95.0% (1129/1188)	15.7% (242/1545)	50.2% (1371/2733)	15.2 (14.1, 16.6)	95.2% (239/251)	19.2% (63/328)	52.2% (307/579)
Diagnosis of HS > 33%								
With 95% specificity	- 2.1 (- 2.9, - 1.2)	64.0% (165/258)	95.0% (2358/2475)	92.0% (2523/2733)	- 3.9 (- 4.4, 0.8)	90.0% (27/30)	97.6% (536/549)	97.2% (563/579)
With 95% sensitivity	7.6 (6.0, 9.0)	95.3% (246/258)	54.3% (1344/2475)	58.2% (1590/2733)	1.6 (- 4.4, 1.8)	96.7% (29/30)	91.1% (500/549)	91.3% (529/579)

Unless otherwise specified, data are percentages, with the number of subjects used to calculate the percentage in parentheses. Percentages were rounded *HS* hepatic steatosis

\*Data are CT<sub>L-S</sub> cut-off values, and data in parentheses are 95% confidence intervals. Dual CT<sub>L-S</sub> cut-off values were determined for either a highly specific diagnosis of HS (with 95% specificity) or a reliable elimination of HS (with 95% sensitivity)

# CT thresholds

- Threshold 48HU on non-con CT
- 100% specific (PDF<sub>FF</sub> ≥ 30%)
- ~ 55% sensitivity
- L-S difference -19 on non-con CT
- optimal for ≥ 30% steatosis



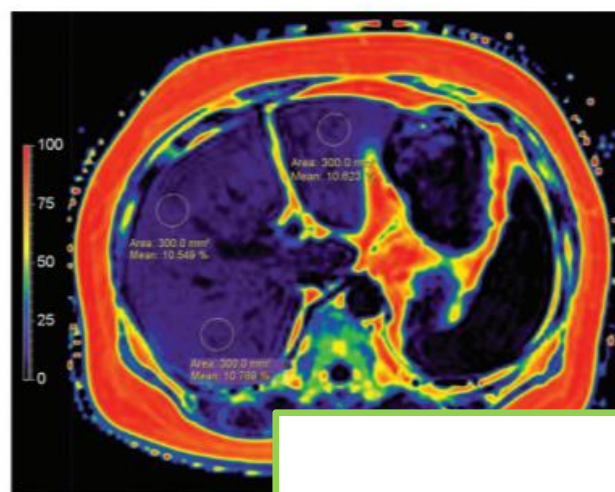
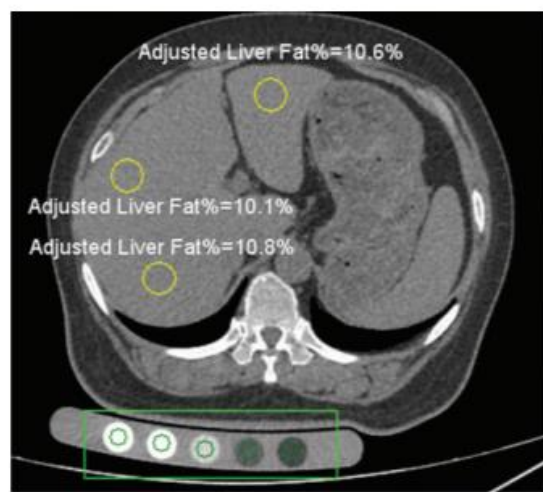
[https://en.wikipedia.org/wiki/Rotary\\_dial](https://en.wikipedia.org/wiki/Rotary_dial)

What is on the horizon?



## Liver Fat Content Measurement with Quantitative CT Validated against MRI Proton Density Fat Fraction: A Prospective Study of 400 Healthy Volunteers

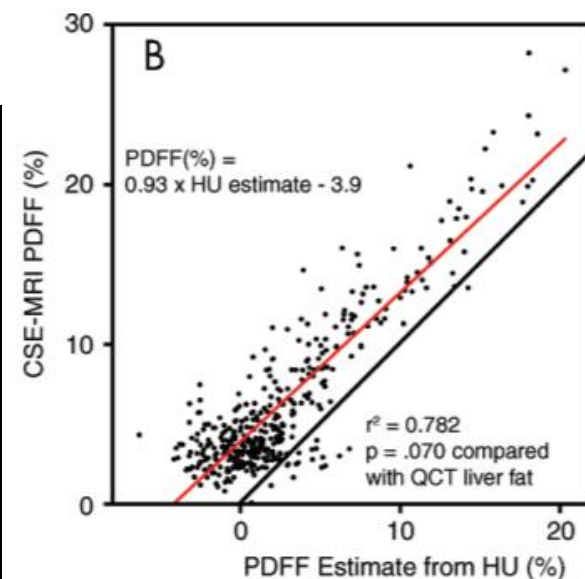
Zhe Guo, MD • Glen M. Blake, PhD • Kai Li, MD • Wei Liang, BS • Wei Zhang, BS • Yong Zhang, MD • Li Xu, MD • Ling Wang, MD • J. Keenan Brown, PhD • Xiaoguang Cheng, MD • Perry J. Pickhardt, MD



a.

b.

**Figure 1:** Liver fat content measurement with (a) quantitative CT and (b) chemical shift MRI in a healthy woman. Three regions of interest (ROIs) were placed in the peripheral areas of the left posterior lobe of the liver, and the average of the three ROIs was chosen for the liver fat



$$\text{Adjusted quantitative CT liver fat} = \left( \frac{CTFF'}{CTFF' + \alpha(1 - CTFF')} \right)$$

# What about DECT?

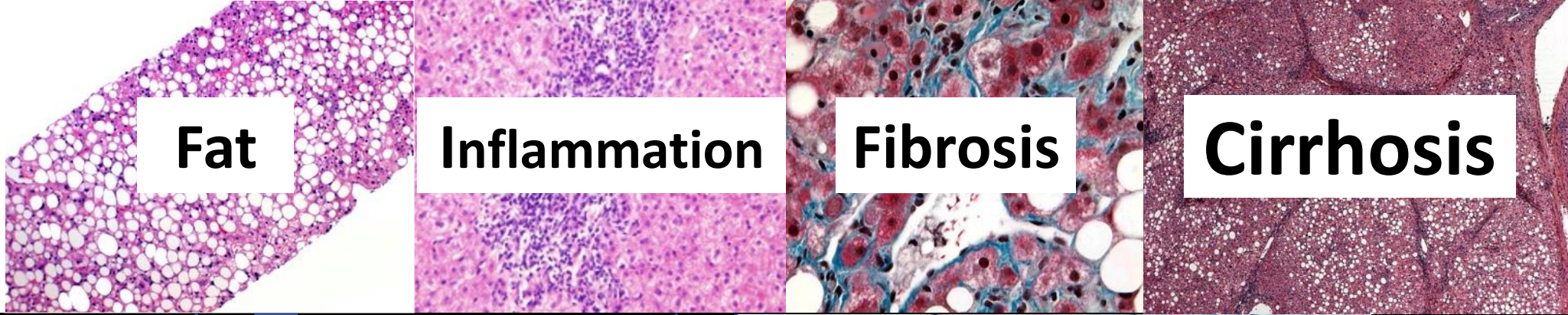
- may add value with virtual non-con
- -otherwise, **no clear advantage** over simple HU measures



**MASLD**

**MASH**

- Ethnicity
- Obesity
- DNA
- T2DM
- Met Sx



**Fat**

**Inflammation**

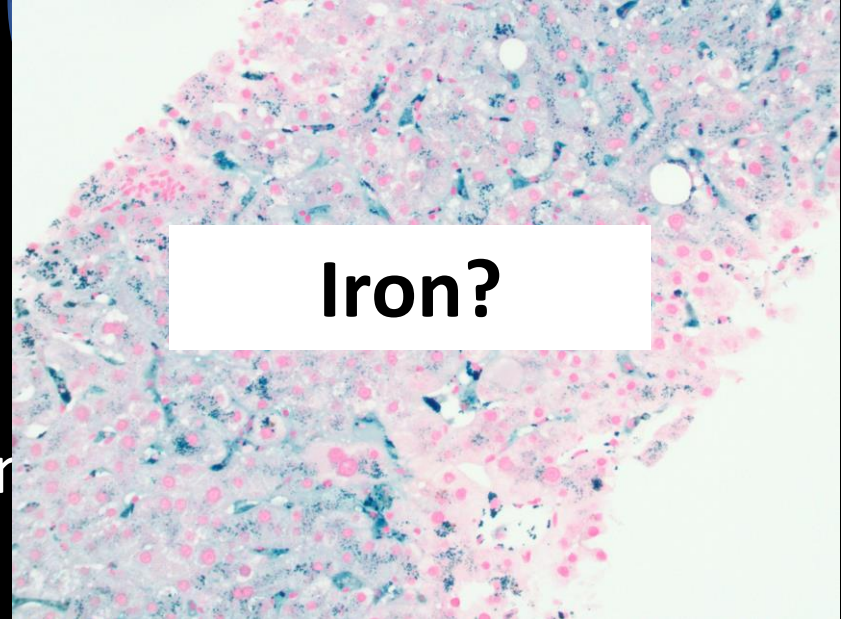
**Fibrosis**

**Cirrhosis**

Lipogenesis

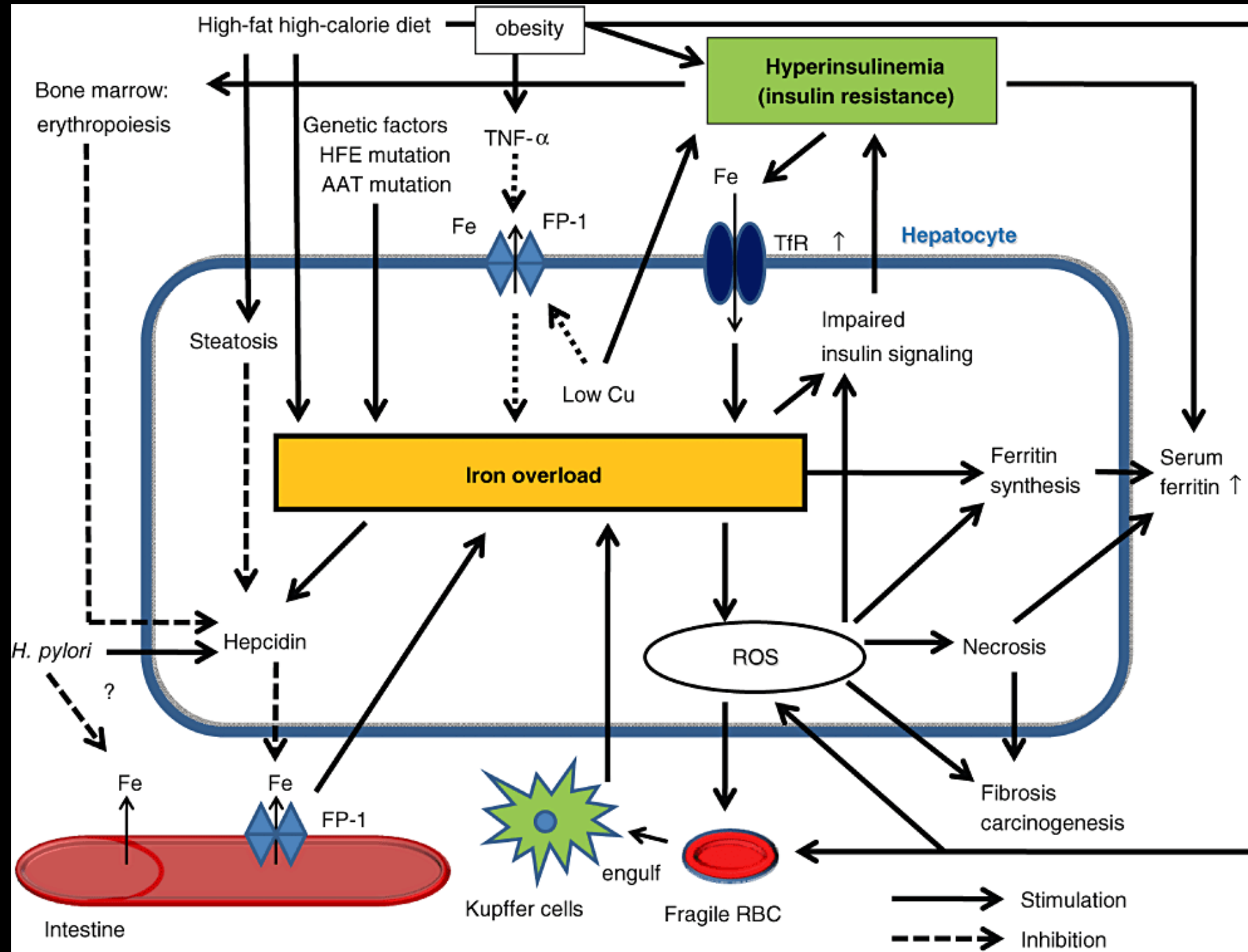
Oxidative stress  
Apoptosis  
Cytokine activation

**Iron?**

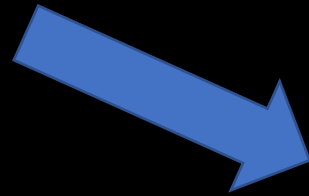


# Iron in MASH

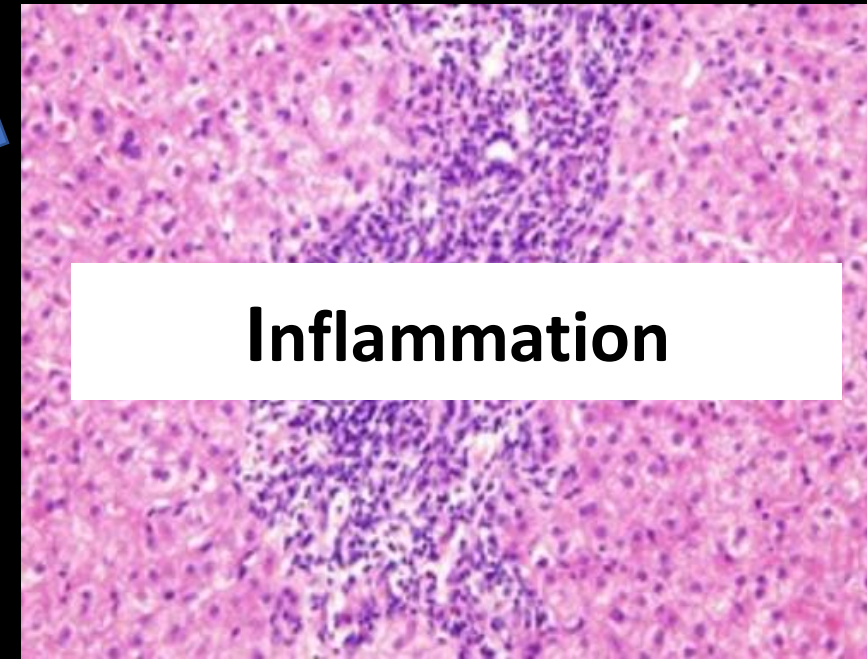
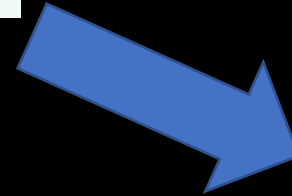
- Uptake in liver increases in MASLD



- Obesity
- DNA
- T2DM
- Met Sx



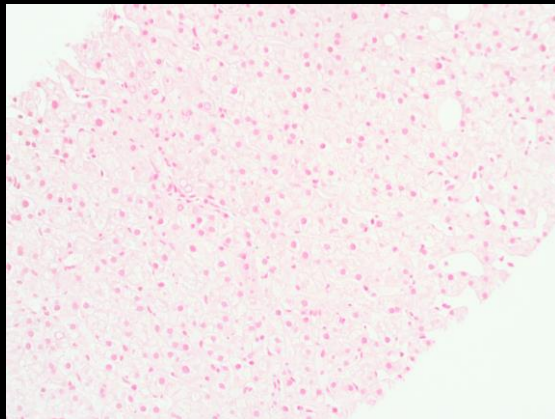
Oxidative stress  
Apoptosis  
Cytokine activation



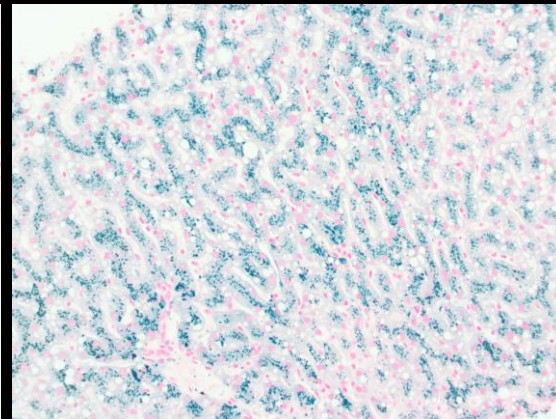
Iron may be a co-factor  
exacerbating oxidative stress!

# Liver Iron

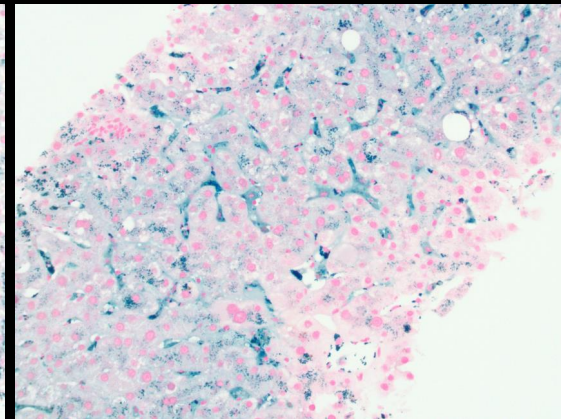
- Iron overload is excess iron in:
  - *hepatocytes*
  - *kupffer cells*
  - *or both*



No Iron

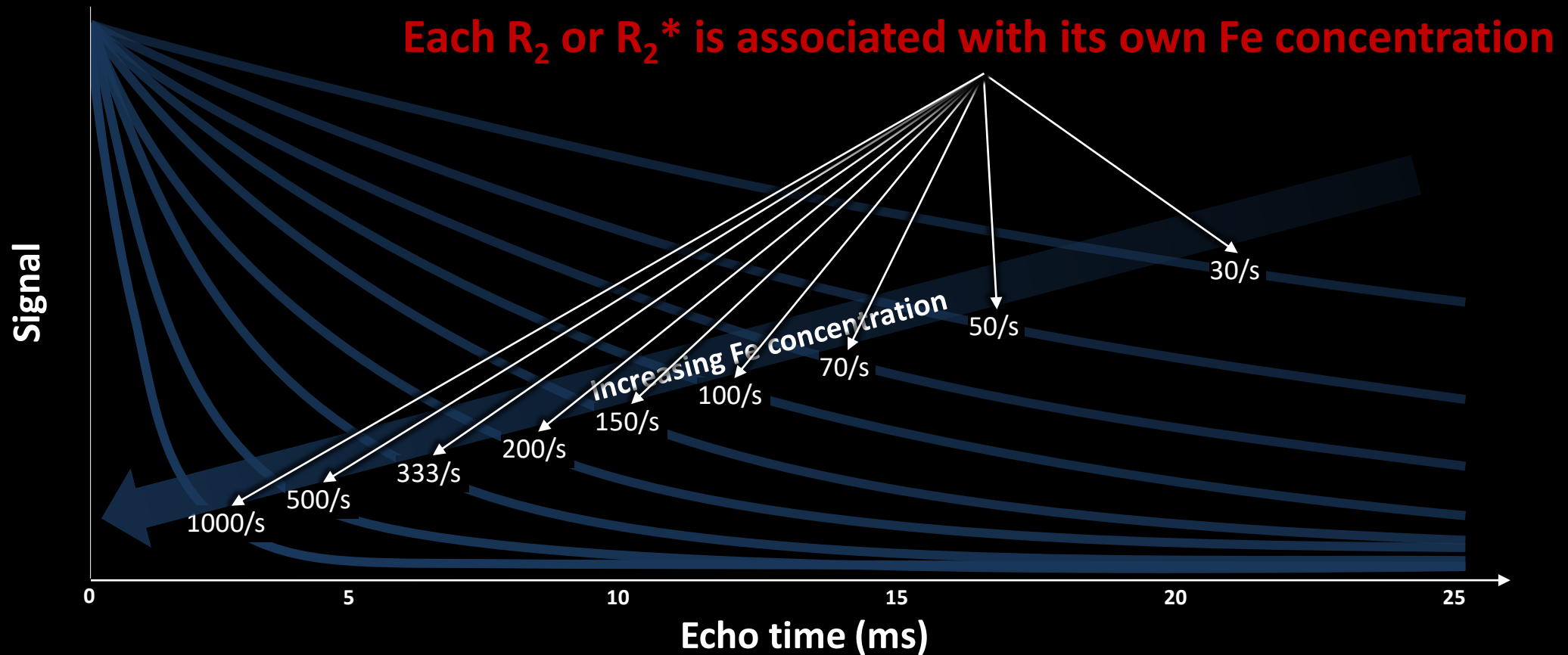


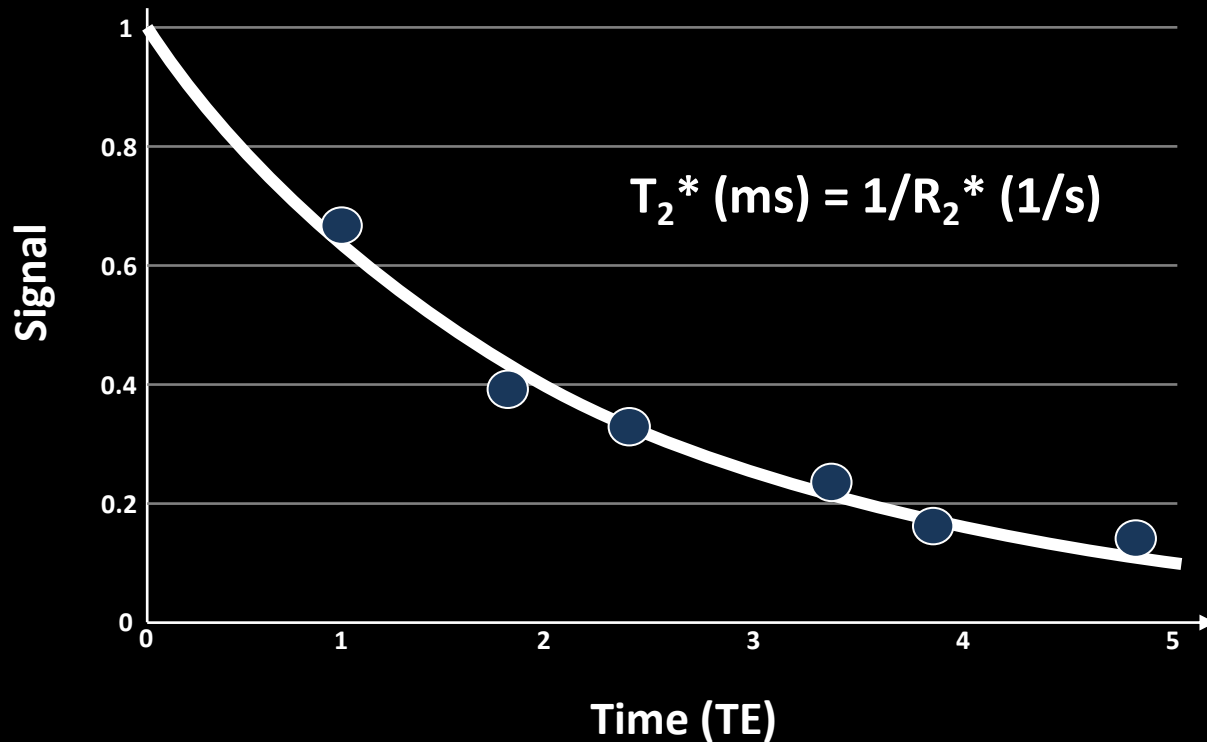
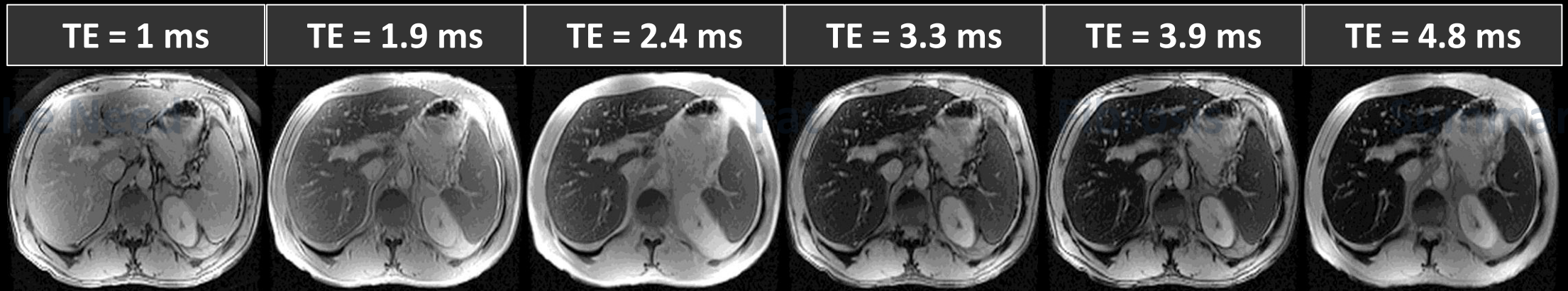
Iron in hepatocytes



Iron in Kupffer cells

As **Fe** increases,  $R_2^*$  increase



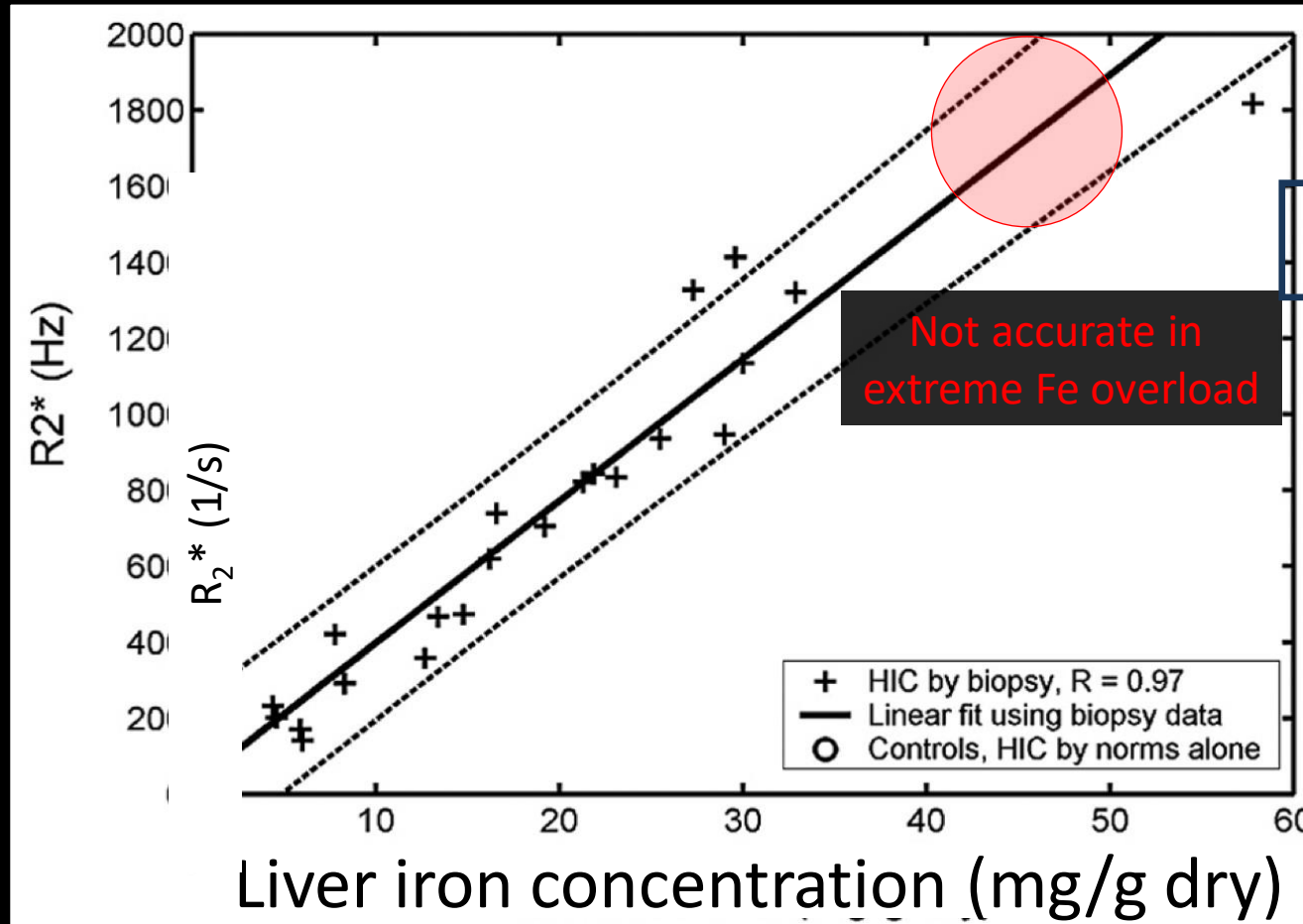


## Modeling:

$R_2^*$  computed from  
observed signal decay

Many modeling  
approaches (beyond scope)

# $R_2^*$ is Biomarker of Fe Overload

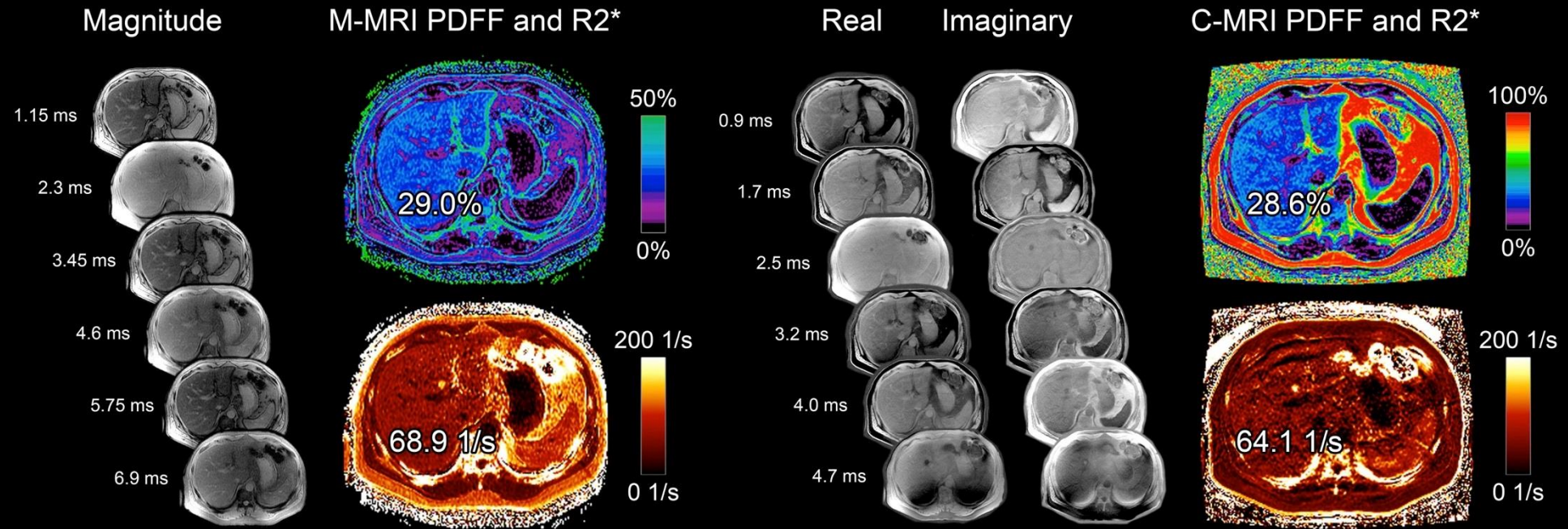


$$[Fe] = -0.63 + 0.0267R_2^*$$

Not accurate in  
extreme Fe overload

Calibration  
Line

# PDFF: $R_2^*$ Map For Free

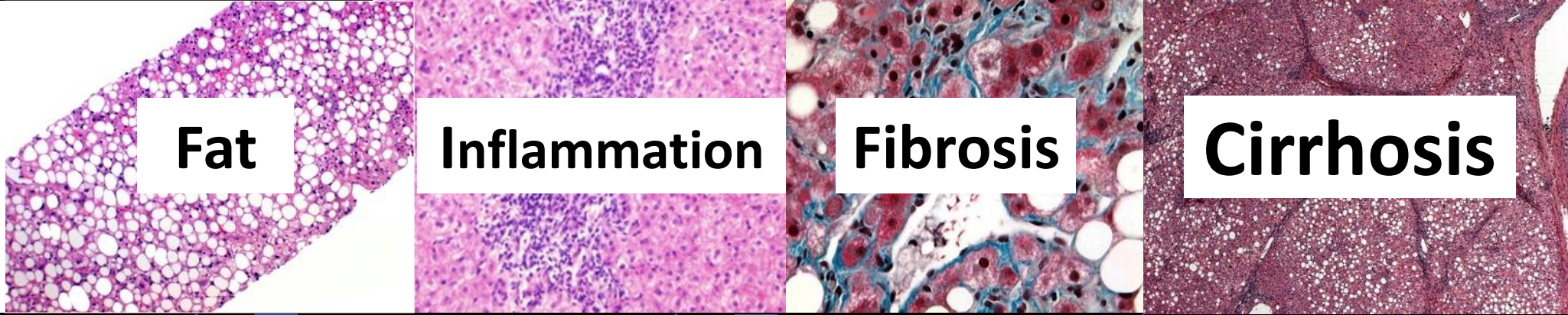




**MASLD**

**MASH**

- Ethnicity
- Obesity
- DNA
- T2DM
- Met Sx



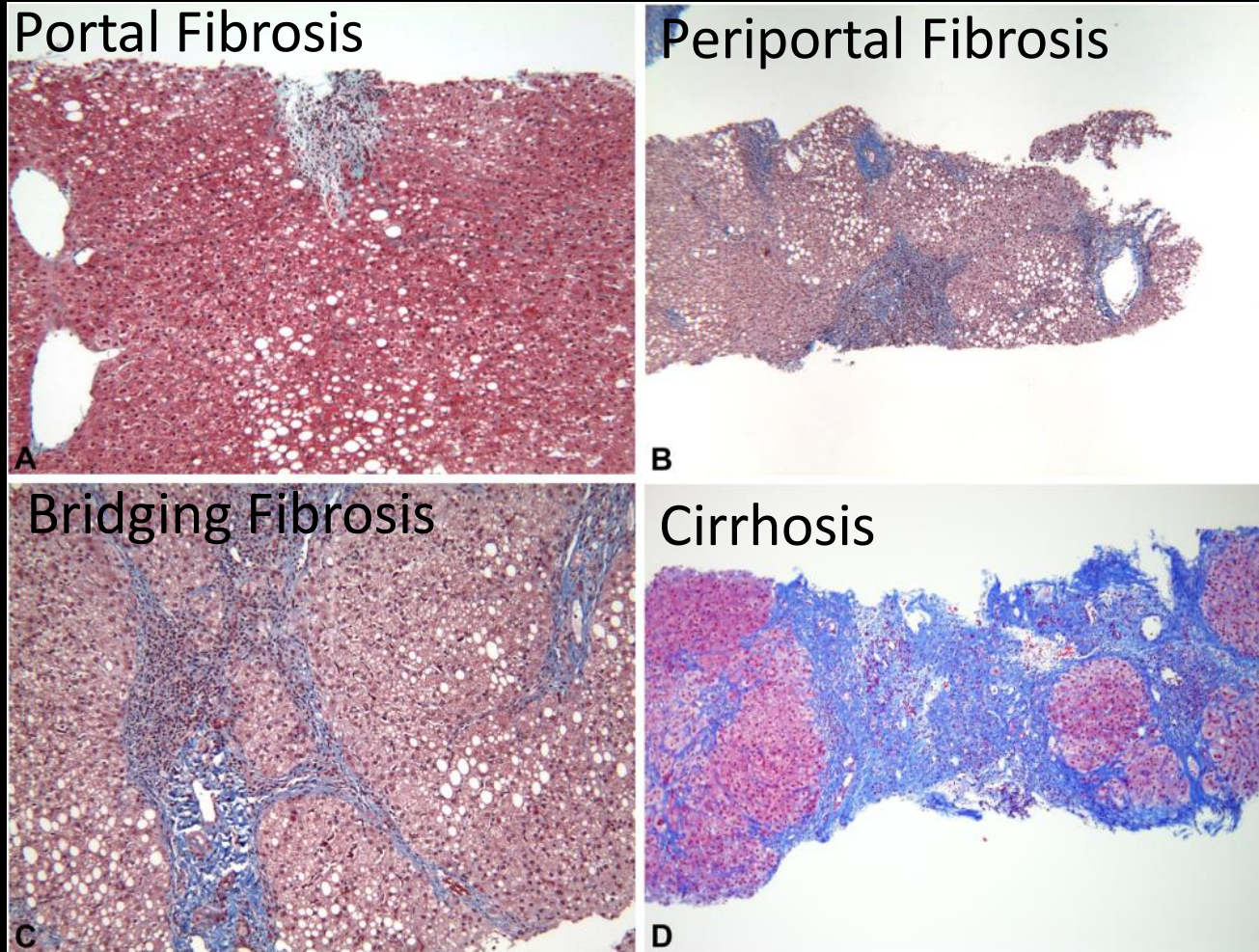
Lipogenesis

Oxidative stress  
Apoptosis  
Cytokine activation

Progressive damage  
Scarring

# Quantifying Fibrosis

# Histology



Stage 1

Stage 2

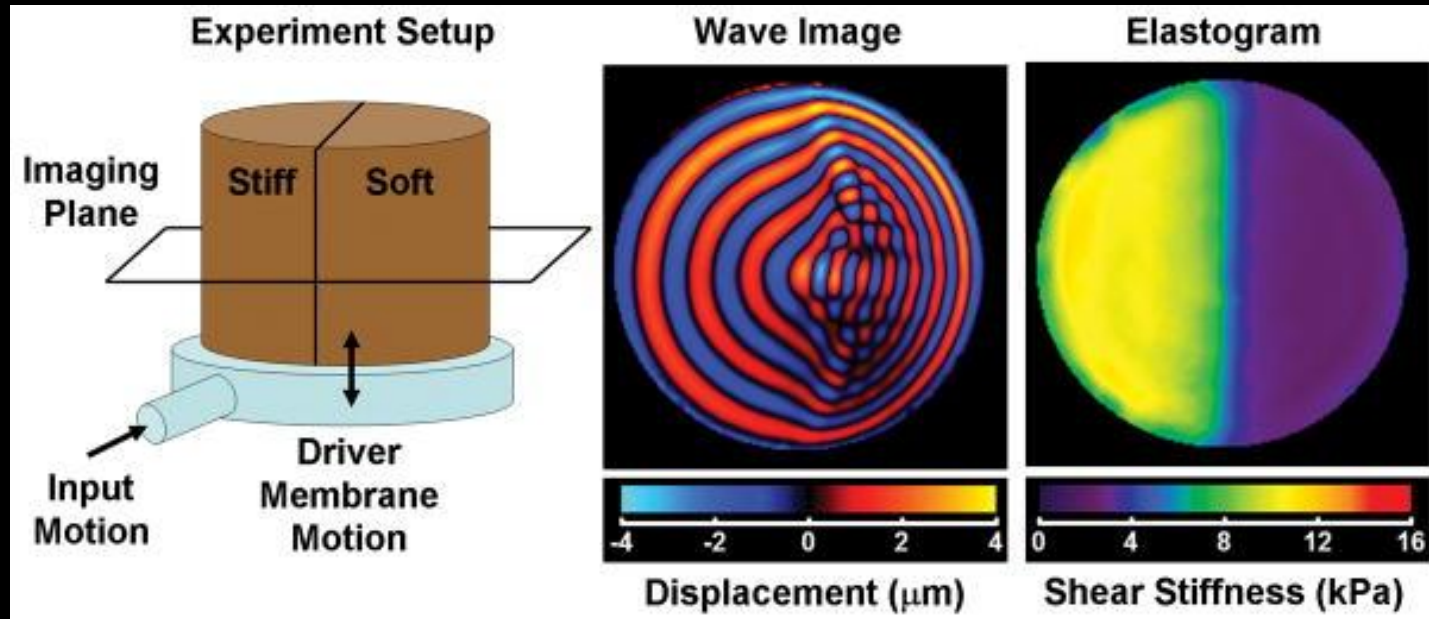
Stage 3

Stage 4

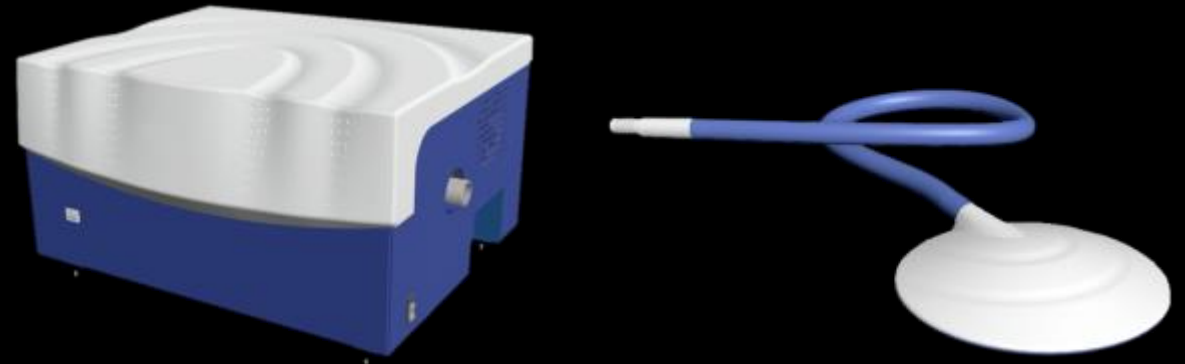
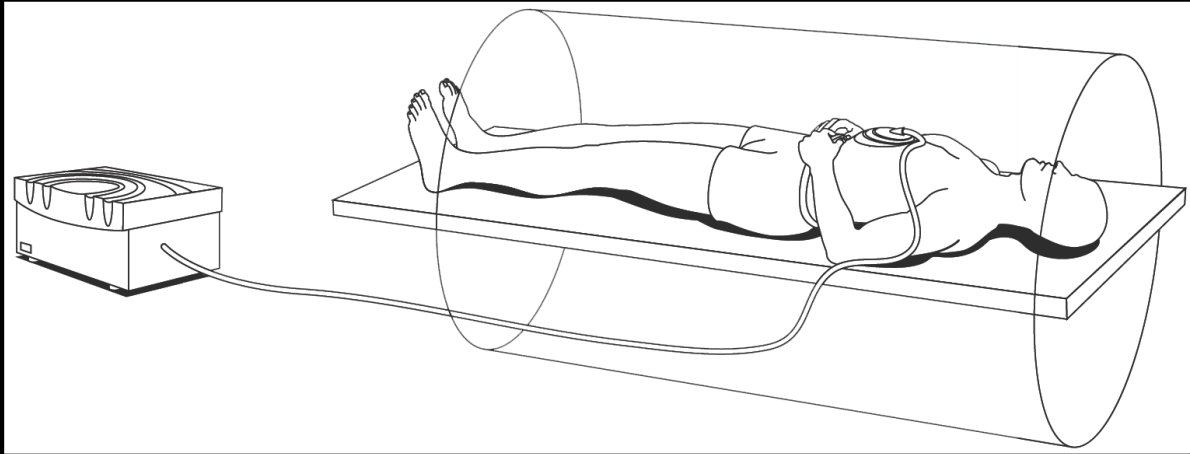
Courtesy of Elizabeth Brunt, M.D.

How do we quantify fibrosis?

# Elastography



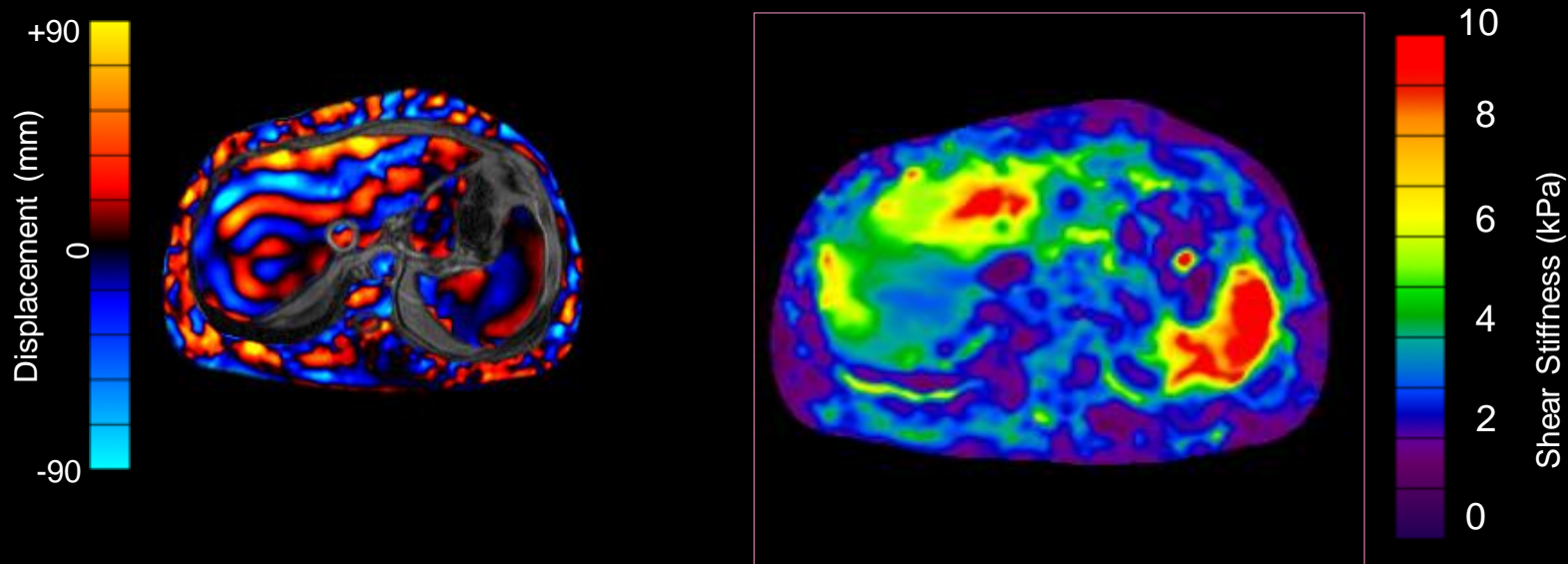
# MRE --- Standardized across vendors



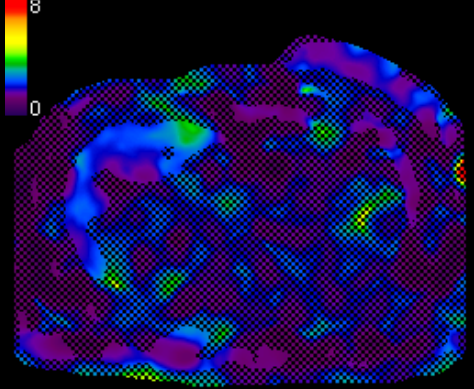
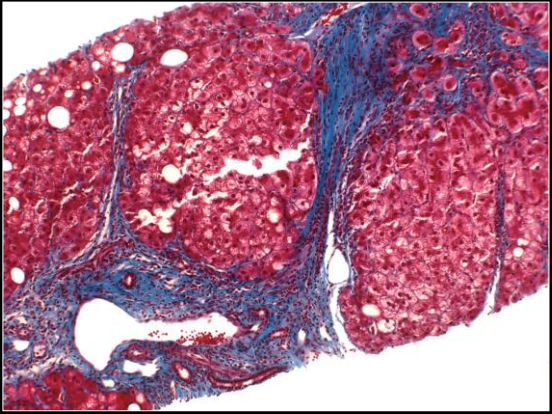
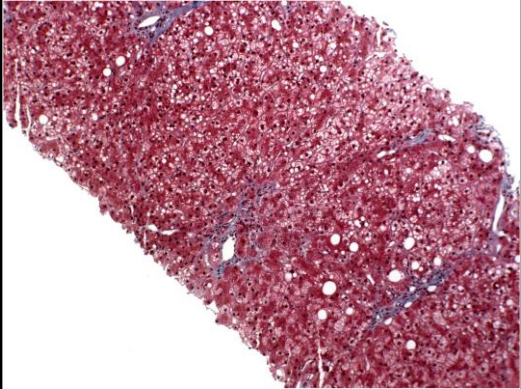
Resoundant

# What are we measuring?

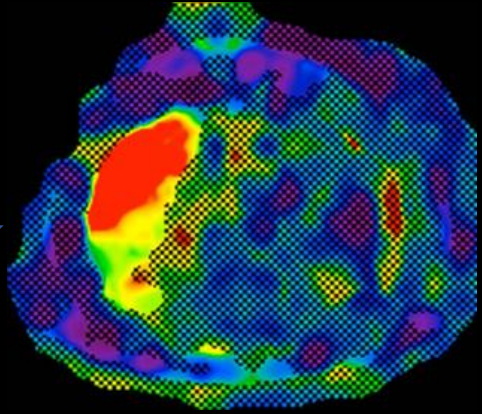
- MRE introduces mechanical waves
- Wave propagation depicted on “Elastogram” via inversion algorithm
  - Shear stiffness (kPa) derived from magnitude of complex shear modulus



Stiffness  
increases with  
stage of fibrosis

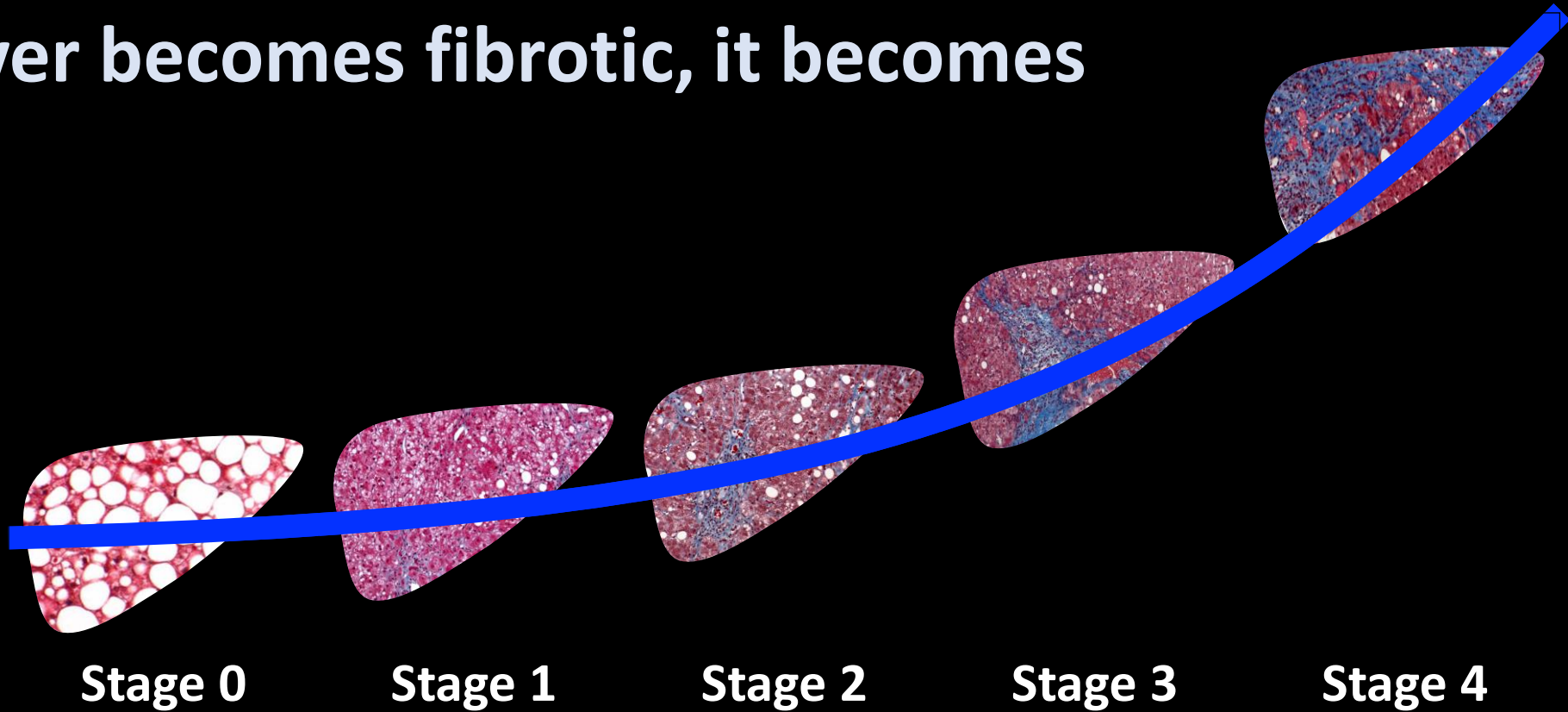


R3.0.3



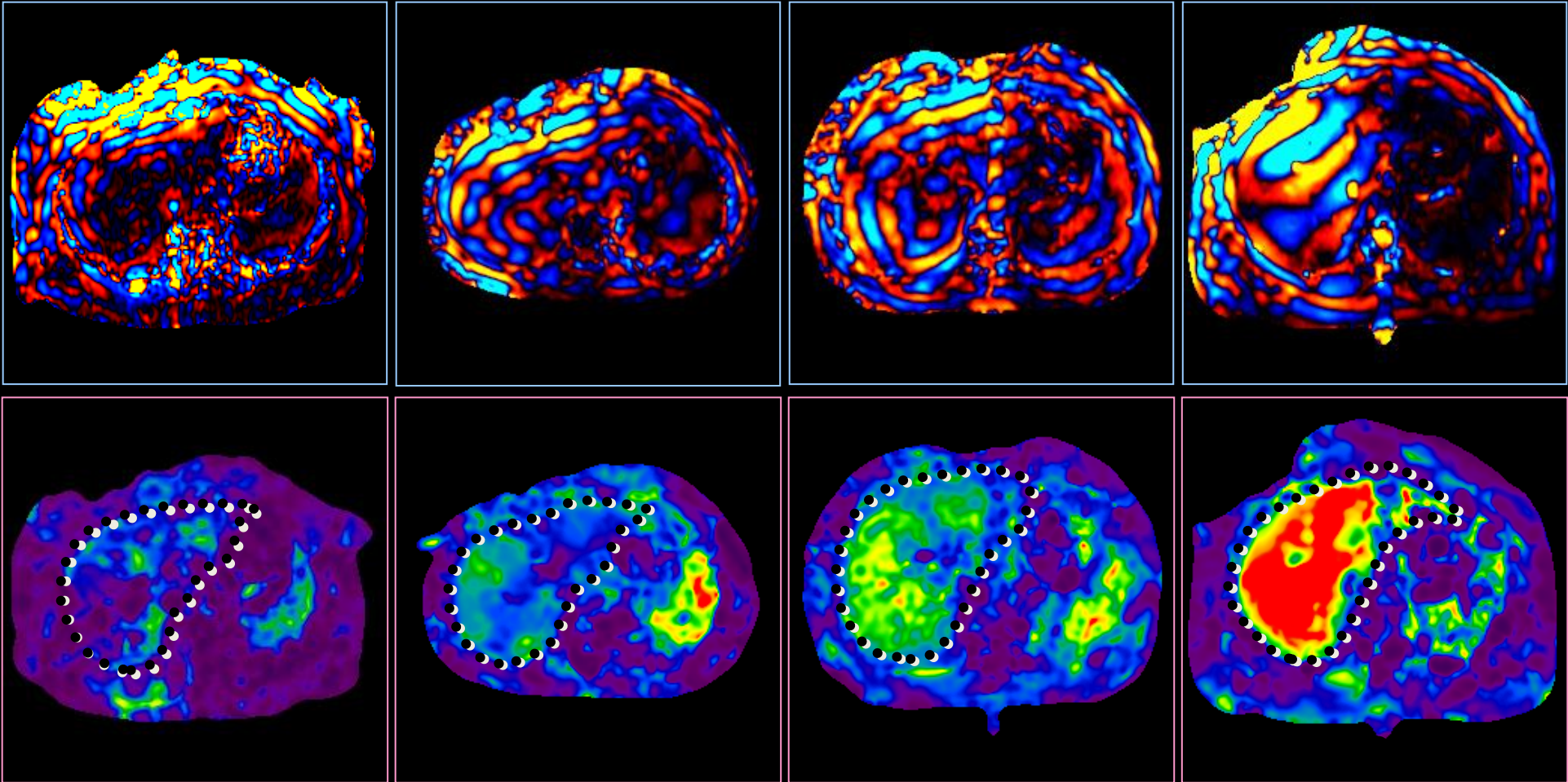
# What is Relationship of stiffness to Fibrosis?

As liver becomes fibrotic, it becomes stiff





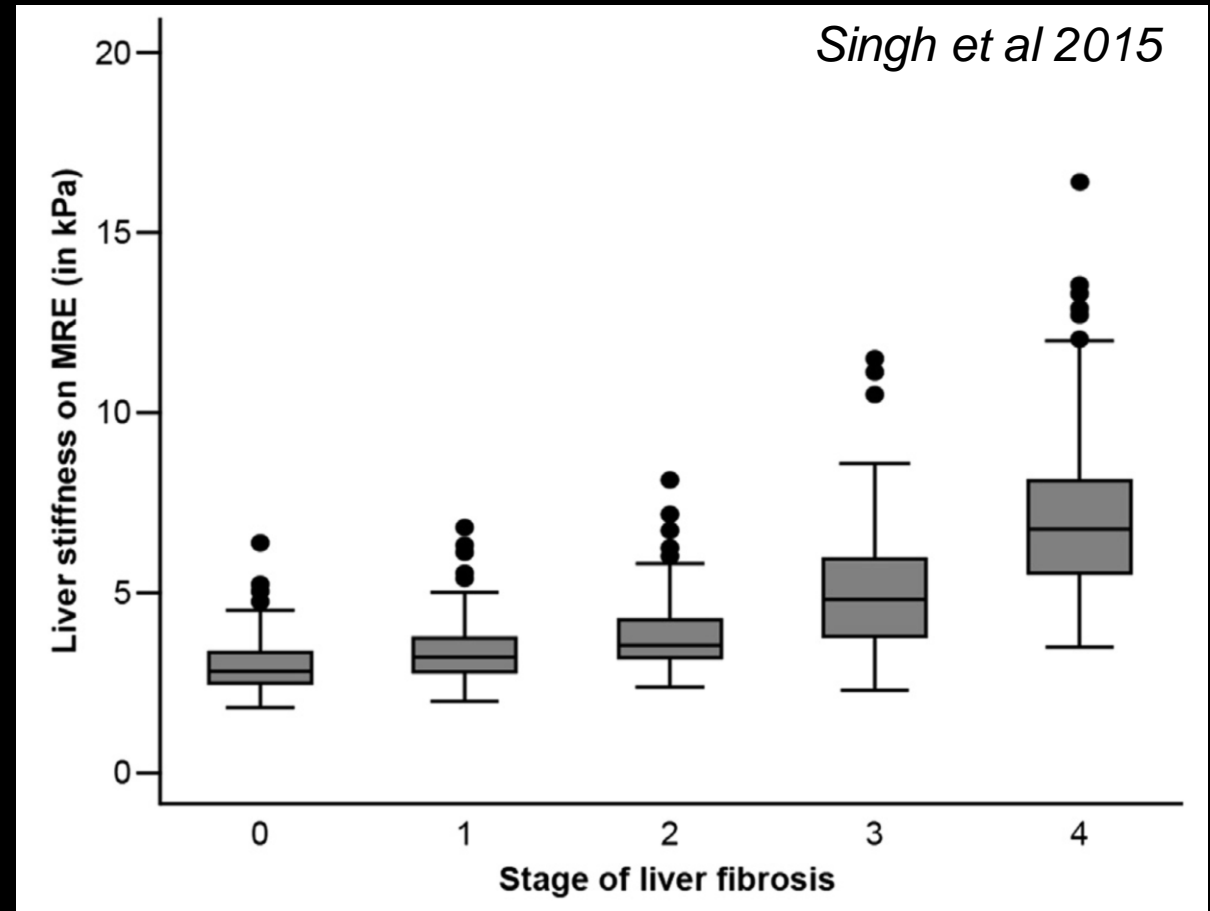
# Liver Fibrosis



Slide courtesy of Claude Sirlin and Dick Ehman, MD

# MRE --- Accurate in cross sectional studies

MRE more accurate than simple noninvasive tests (e.g. FIB-4) for diagnosing advanced fibrosis in NAFLD-Xiao, Hepatology 2017



Meta-Analysis of 12 Studies

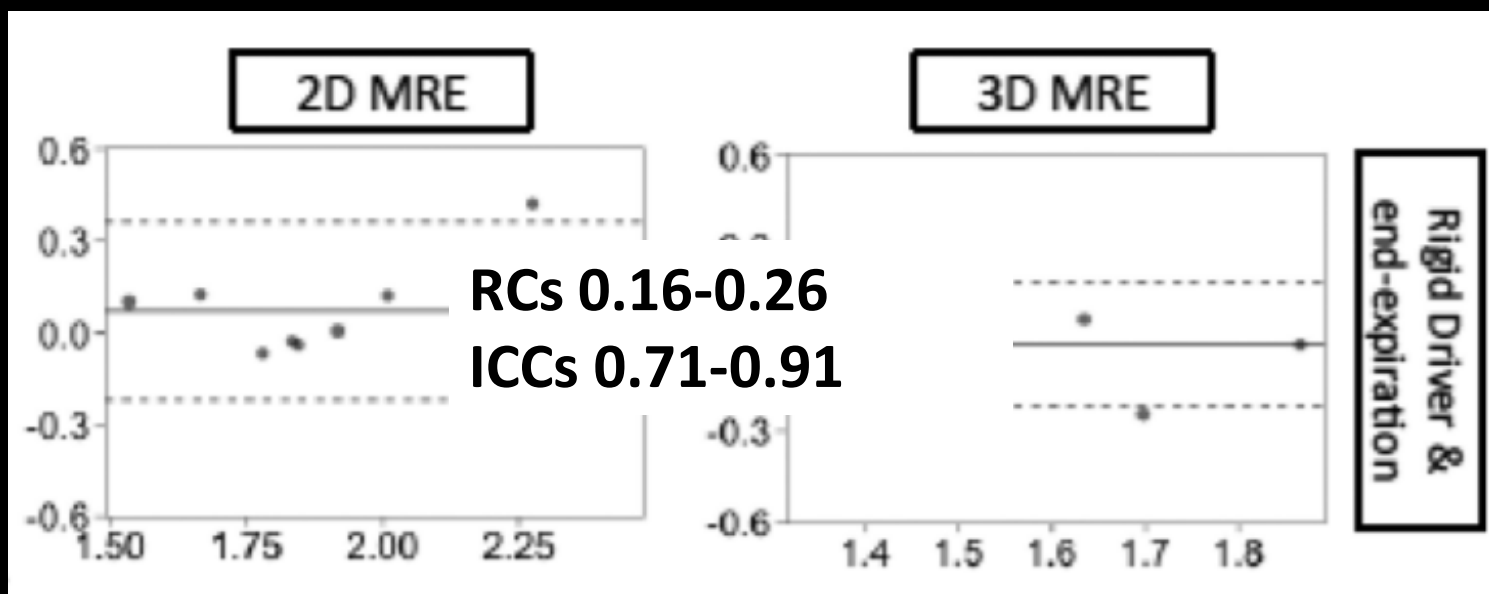
(Individual Participant Data, n=697)

# MRE --- Repeatability/Reproducibility?

Stay Tuned for Definitive work on this: Nimble 1.2: Work in progress!

## Normal volunteer repeatability

Within subject  
coefficient of  
variation  $\sim 7\%$



Quantitative  
Imaging  
Biomarkers  
Alliance

RSNA<sup>®</sup>

Change in stiffness of  $\geq 19\%$  represents a true change with 95% certainty

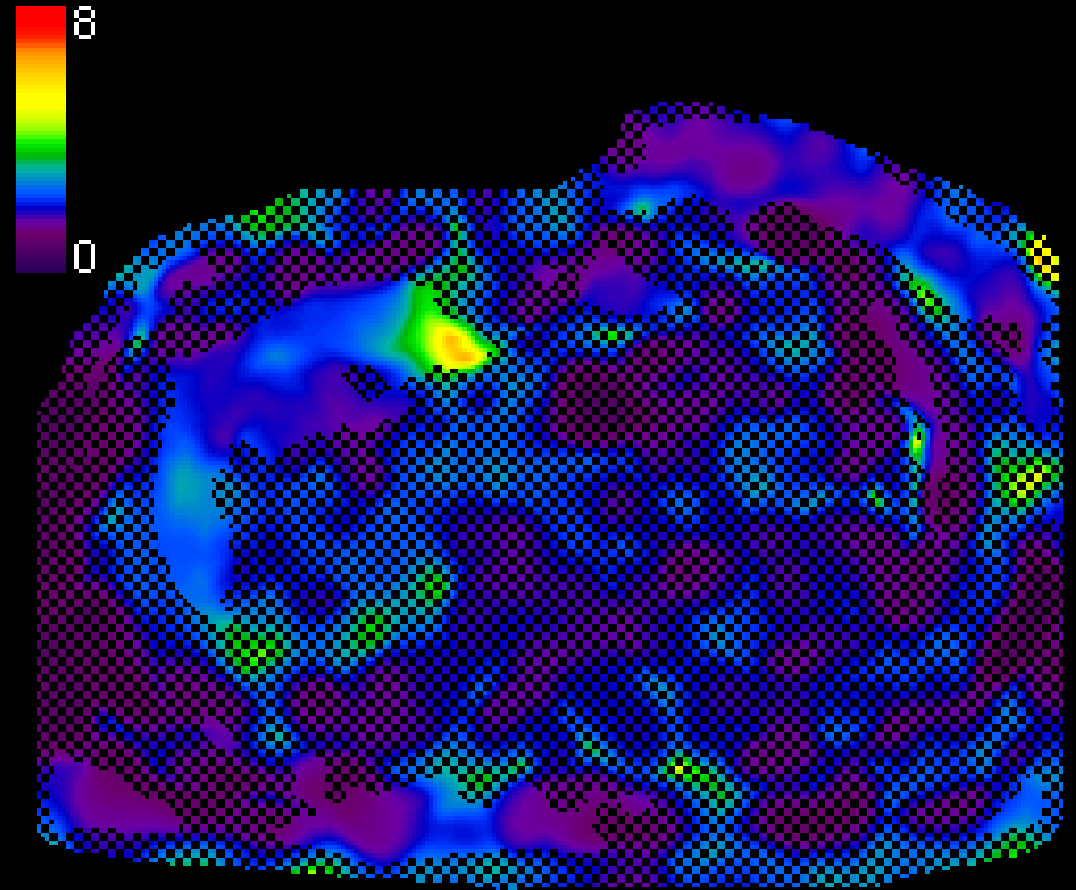
RC 2.77 x wCV=19%



MRE profile

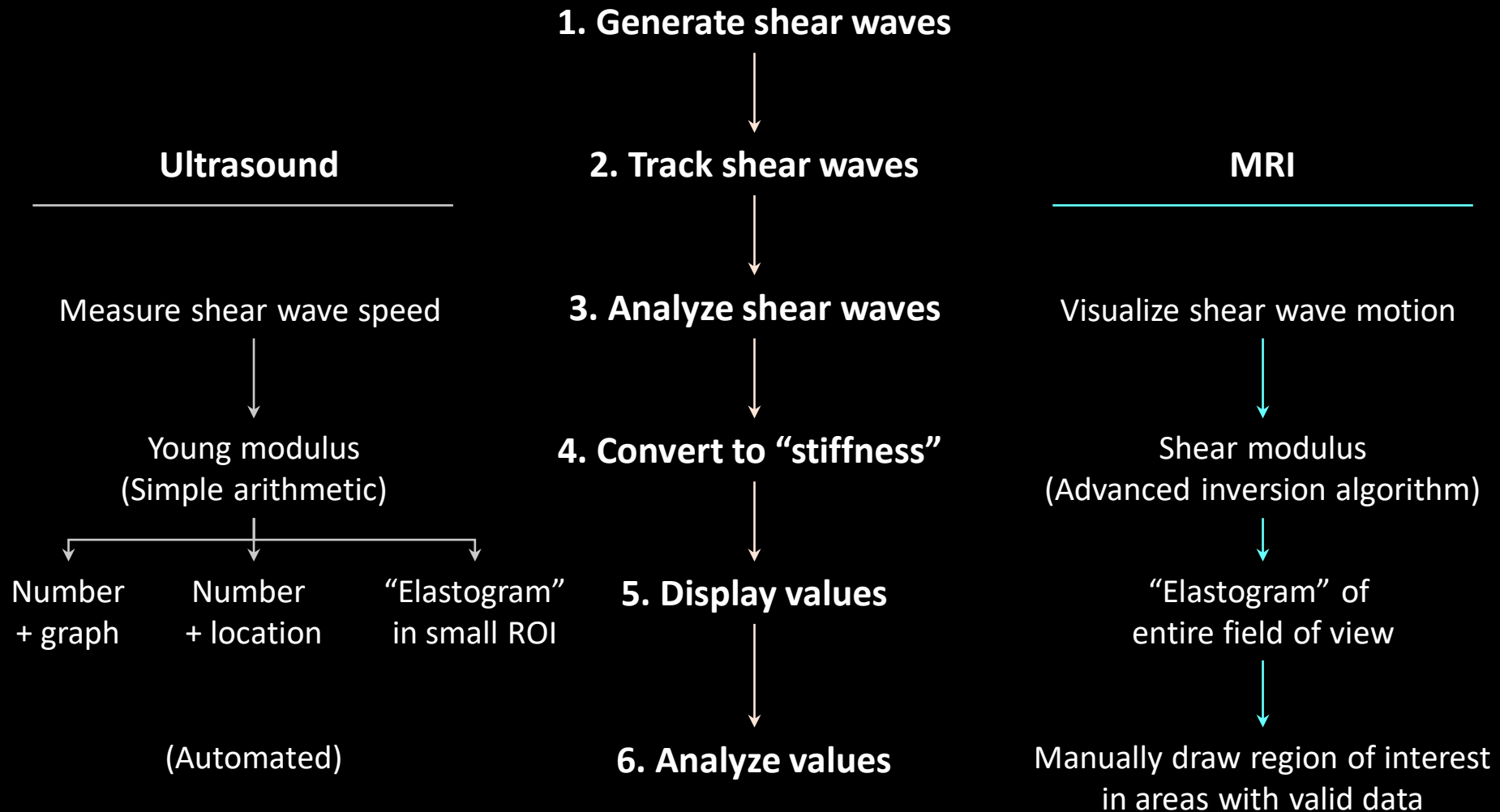
# Elastography

- **MRI-**
- 2D (*and 3D elastography*)
  
- **Ultrasound-**
- Transient elastography
- Point shear wave
- 2D shear wave



R3.0.3

# Elastography broken down

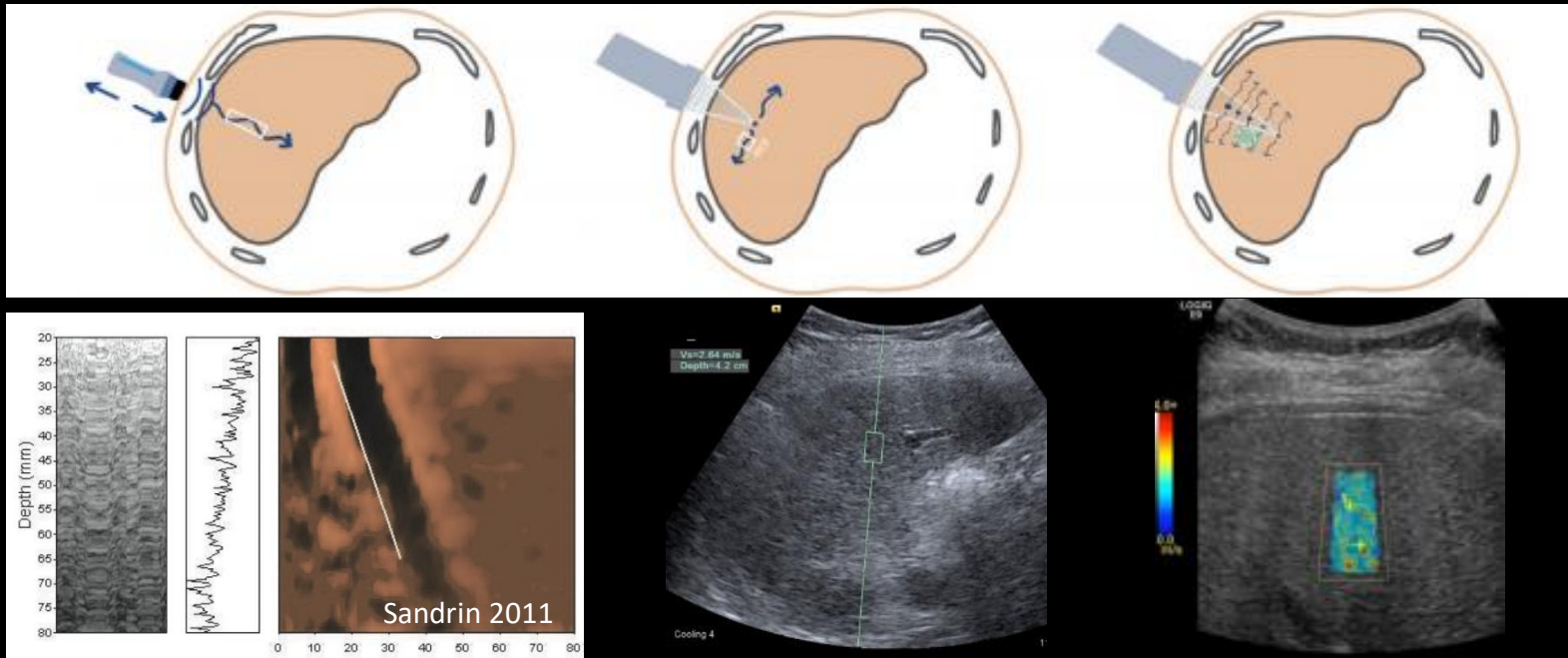


# US Elastography varieties

Vibration controlled  
Transient (VCTE;  
Fibroscan)

Point Shear  
Wave (PSW)

2D Shear Wave  
(2D SWE)



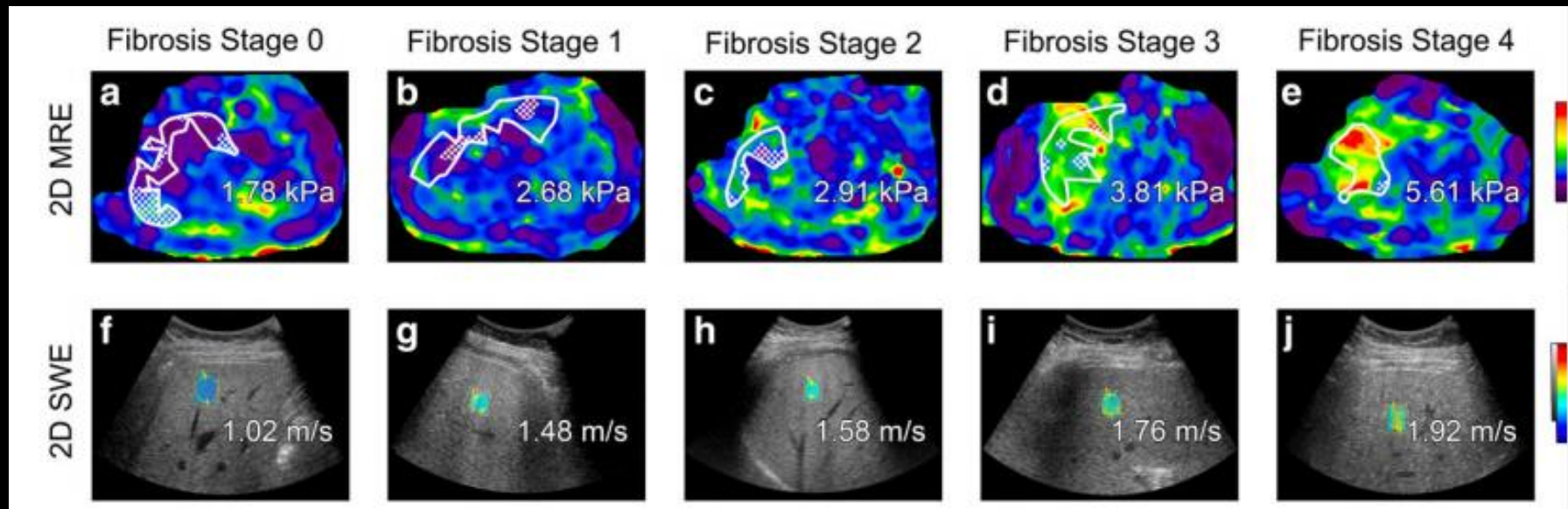
# Summary of US accuracy

- All are potentially impacted by obesity
- Poor for early fibrosis (Stage 1 vs. 2)
- OK for Stage  $\geq 2$  (AUCs 0.62-0.91)
- Excellent for detecting Stage 4 (AUCs 0.80-0.97)
  
- No consensus on which is most accurate  
pSWE/2D SWE > VCTE
- Results between vendors/methods may differ



# US vs. MR Elastography

- **MRE slightly more accurate**, especially at lower stages
- Stage > 2 MRE AUCs 0.89-0.93 v. US 0.81-0.91  
Stage > 3 MRE AUCs 0.87-0.96 v. US 0.80-0.90
- Stage > 4 MRE AUCs 0.87-0.95 v. US 0.69-0.92



# Liver Fibrosis Imaging: A Clinical Review of Ultrasound and Magnetic Resonance Elastography

Yingzhen N. Zhang, MD,<sup>1</sup> Kathryn J. Fowler, MD,<sup>1</sup> Arinc Ozturk, MD,<sup>2</sup> Chetan K. Potu, BS,<sup>1</sup> Ashley L. Louie, BA,<sup>1</sup> Vivian Montes, BA,<sup>1</sup> Walter C. Henderson, BA,<sup>1</sup> Kang Wang, MD,<sup>1</sup> Michael P. Andre, PhD,<sup>3</sup> Anthony E. Samir, MD,<sup>2</sup> and Claude B. Sirlin, MD<sup>1\*</sup>

Liver fibrosis is a histological hallmark of most chronic liver diseases, which can progress to cirrhosis and liver failure, and predisposes to hepatocellular carcinoma. Accurate diagnosis of liver fibrosis is necessary for prognosis, risk stratification, and treatment decision-making. Liver biopsy, the reference standard for assessing liver fibrosis, is invasive, costly, and impractical for surveillance and treatment response monitoring. Elastography offers a noninvasive, objective, and quantitative alternative to liver biopsy. This article discusses the need for noninvasive assessment of liver fibrosis and reviews the comparative advantages and limitations of ultrasound and magnetic resonance elastography techniques with respect to their basic concepts, acquisition, processing, and diagnostic performance. Variations in clinical contexts of use and common pitfalls associated with each technique are considered. In addition, current challenges and future directions to improve the diagnostic accuracy and clinical utility of elastography techniques are discussed.

**Level of Evidence:** 5

**Technical Efficacy Stage:** 2

What is on the horizon?

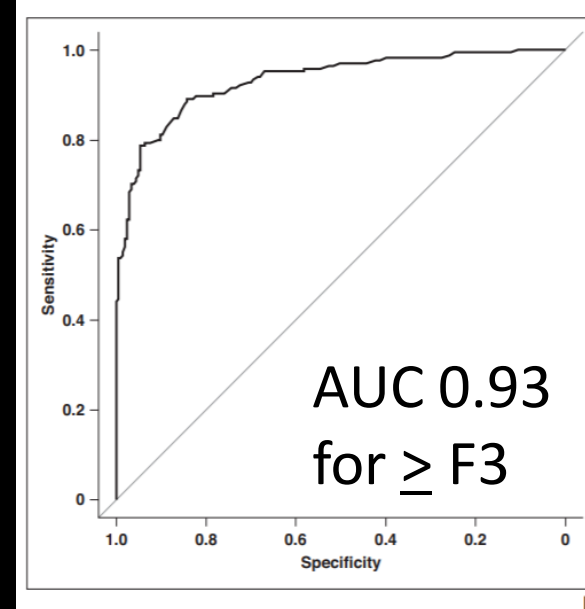
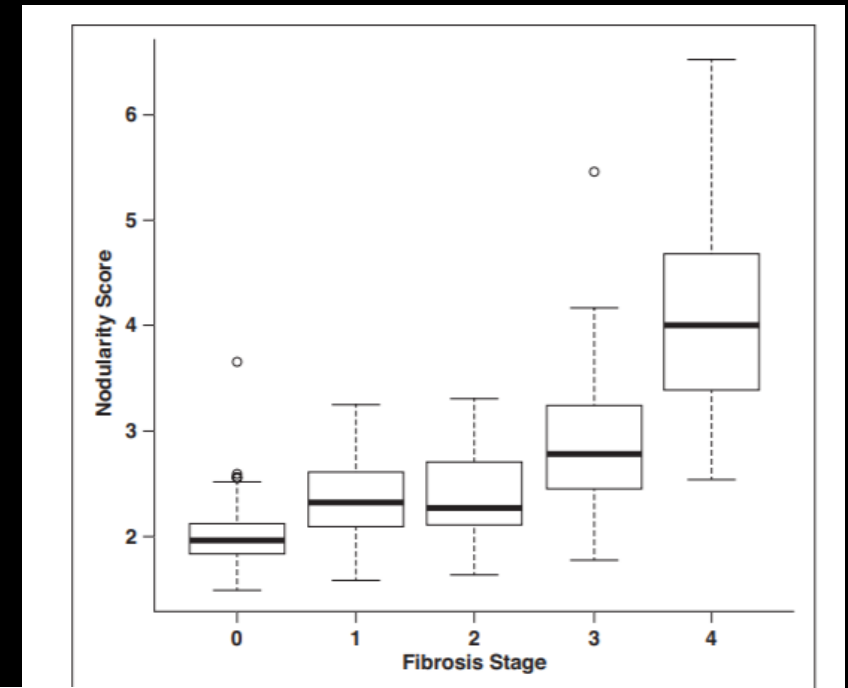
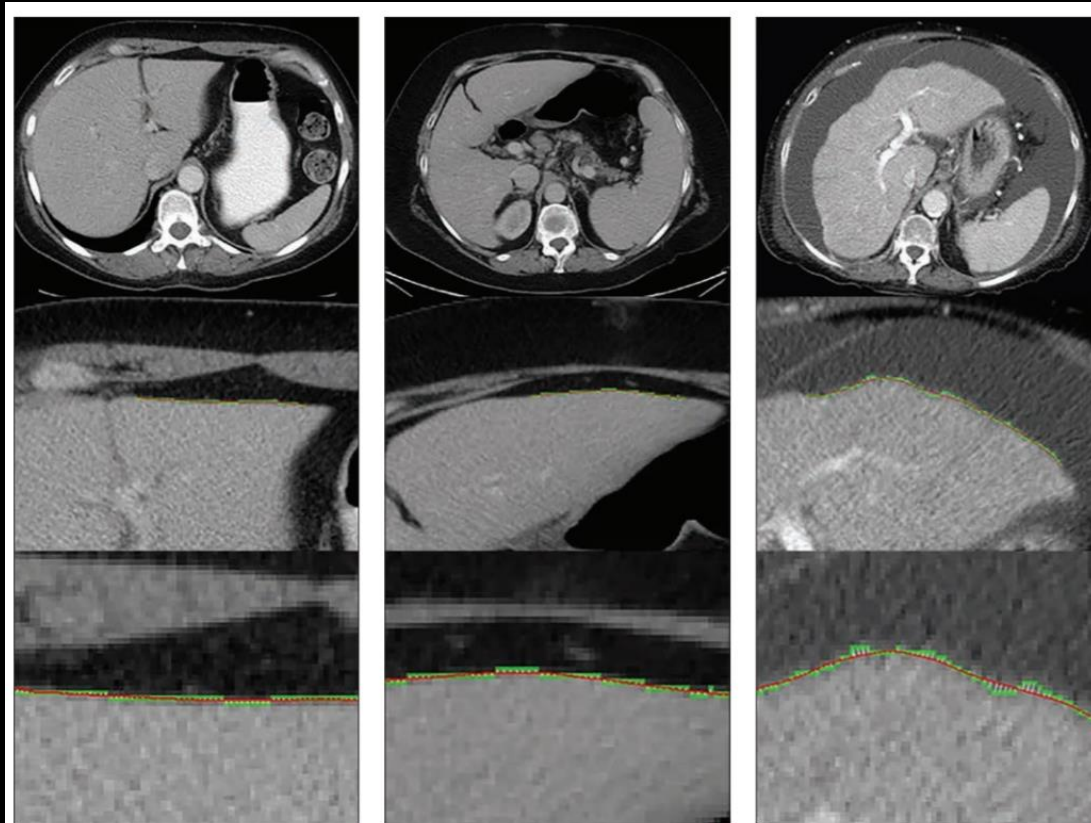


# Accuracy of Liver Surface Nodularity Quantification on MDCT as a Noninvasive Biomarker for Staging Hepatic Fibrosis

Perry J. Pickhardt<sup>1</sup>  
Kyle Malecki  
John Kloke  
Meghan G. Lubner

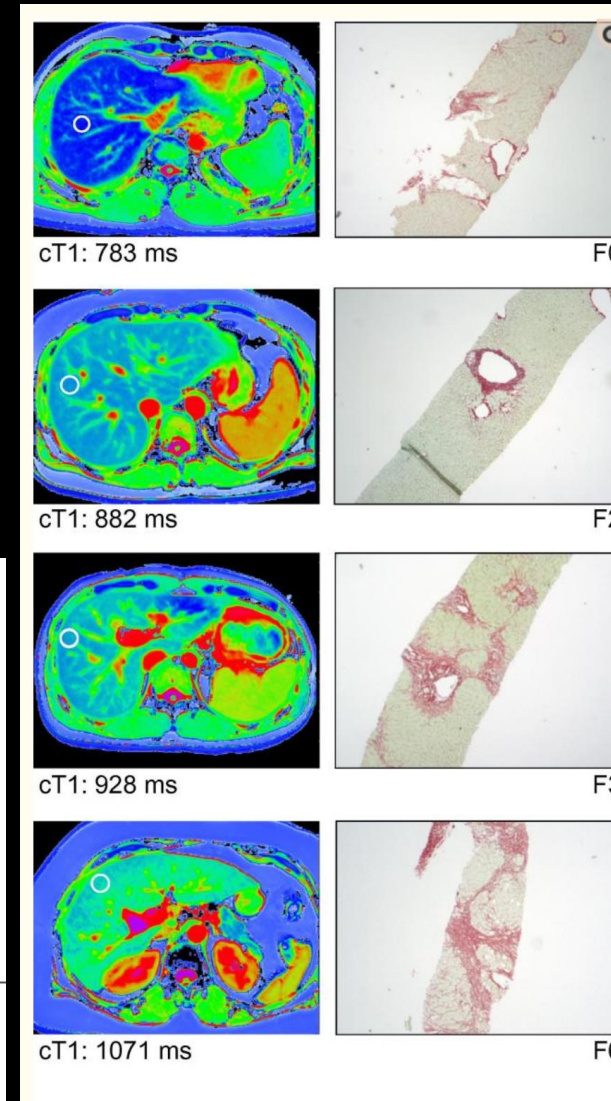
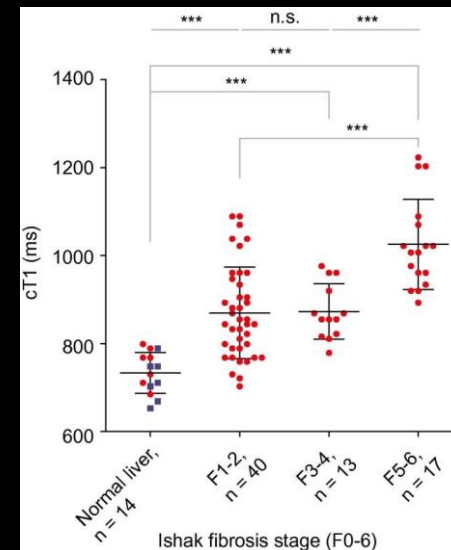
**OBJECTIVE.** The purpose of this study was to investigate objective semiautomated measurement of liver surface nodularity on MDCT for prediction of underlying hepatic fibrosis (stages F0–F4).

**MATERIALS AND METHODS.** Contrast-enhanced abdominal MDCT scans were assessed with an independently validated semiautomated surface nodularity tool. A series of 10 or more consecutive ROI measurements along the anterior aspect of the liver totaling a length



# T1 relaxometry and mapping

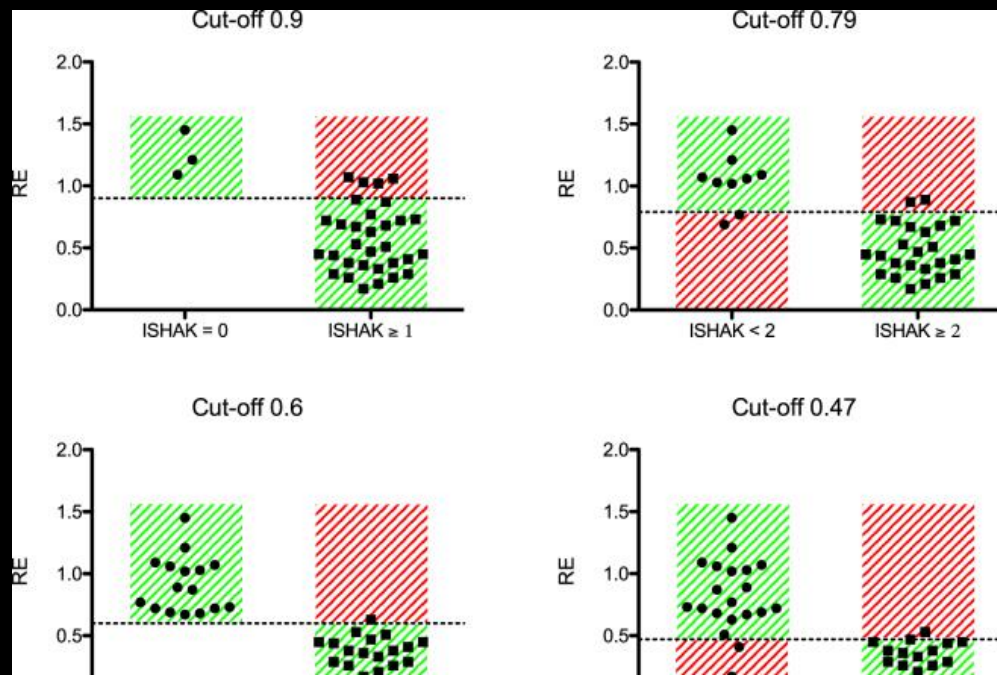
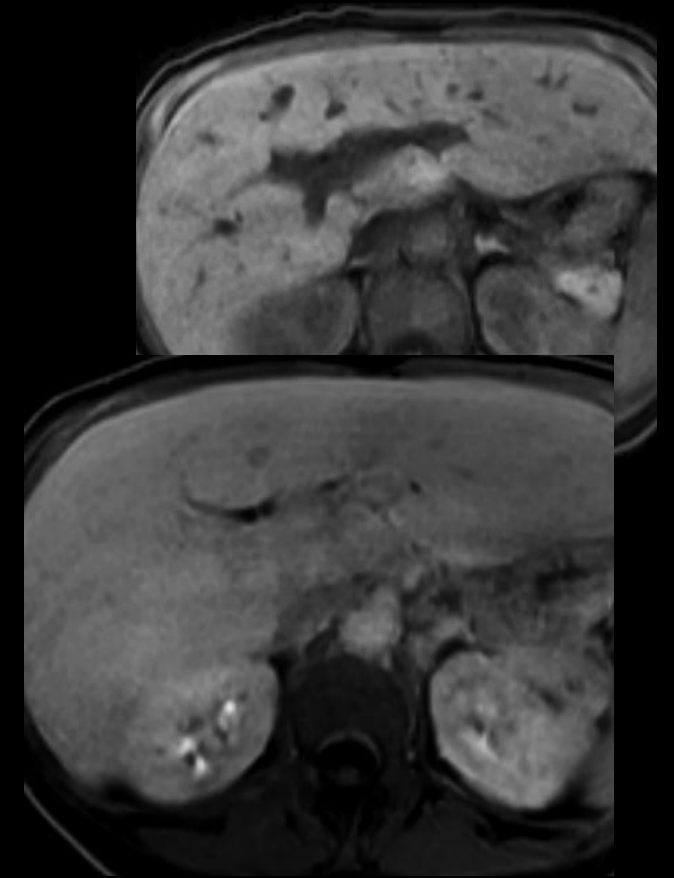
- T1 rho may detect macromolecules in tissue  
collagen and proteoglycans alter T1 relaxation
- Similar to PDFF, must be corrected for confounders (cT1)
- Prelim data promising!



## Detecting liver fibrosis with Gd-EOB-DTPA-enhanced MRI: A confirmatory study

Niklas Verloh,<sup>✉1</sup> Kirsten Utpatel,<sup>2</sup> Michael Haimerl,<sup>1</sup> Florian Zeman,<sup>3</sup> Lukas Beyer,<sup>1</sup> Claudia Fellner,<sup>1</sup> Frank Brennfleck,<sup>4</sup> Marc H Dahlke,<sup>4</sup> Christian Stroszczynski,<sup>1</sup> Matthias Evert,<sup>2</sup> and Philipp Wiggermann<sup>1</sup>

$$\text{Relative enhancement (RE) of signal intensity (SI)} = \frac{SI_{\text{post}} - SI_{\text{pre}}}{SI_{\text{pre}}}$$



**Relative enhancement EOB**

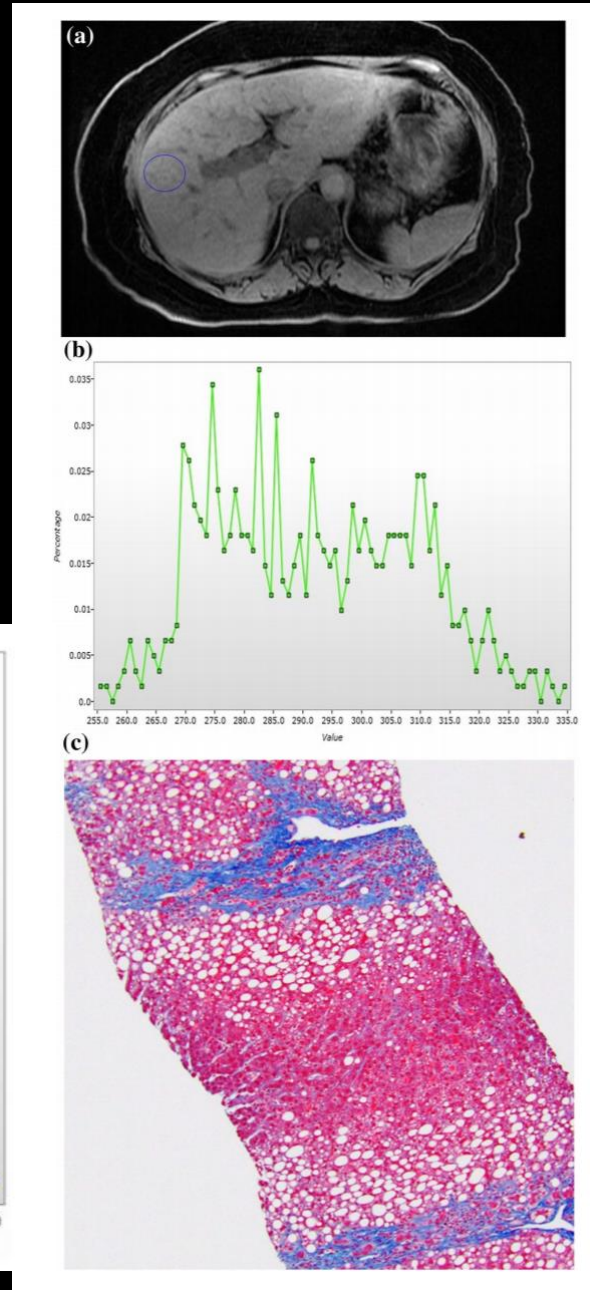
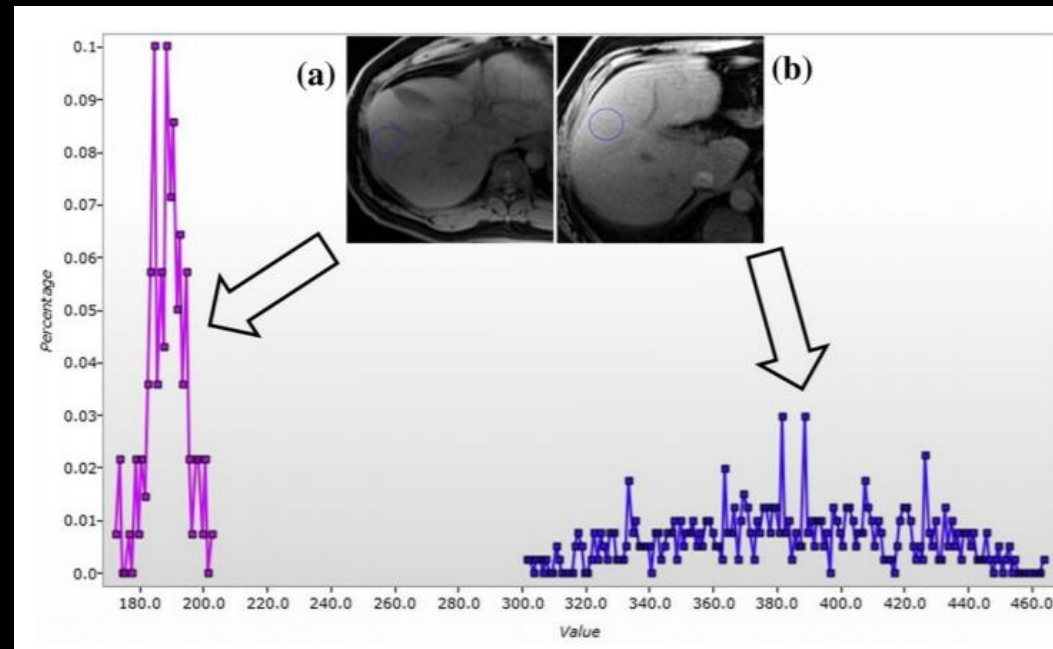
Sensitivity  $\geq 86\%$

PPV  $\geq 86\%$

Correctly classified most patients

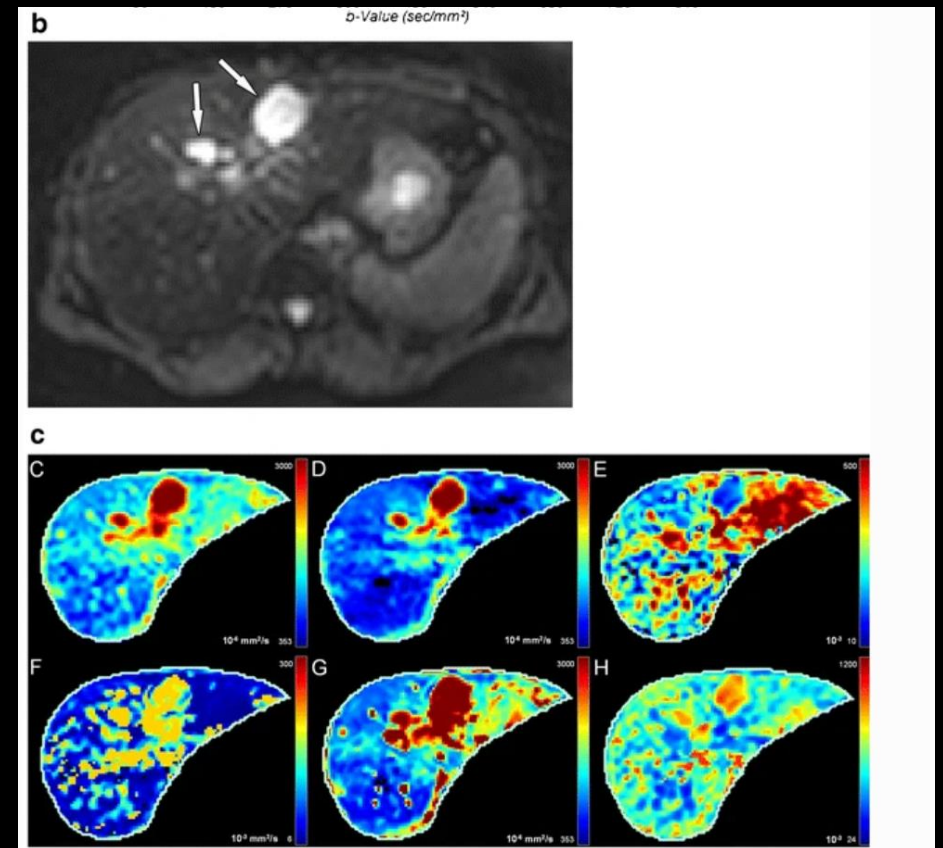
# Texture analysis

- Characterizes spatial variation of gray levels
- Single center studies show some discriminatory ability
- Further testing needed



# Advanced DWI

- Collagen deposition expands extracellular space and alters proton diffusion
- IVIM-intravoxel incoherent motion
- Prelim studies show some potential

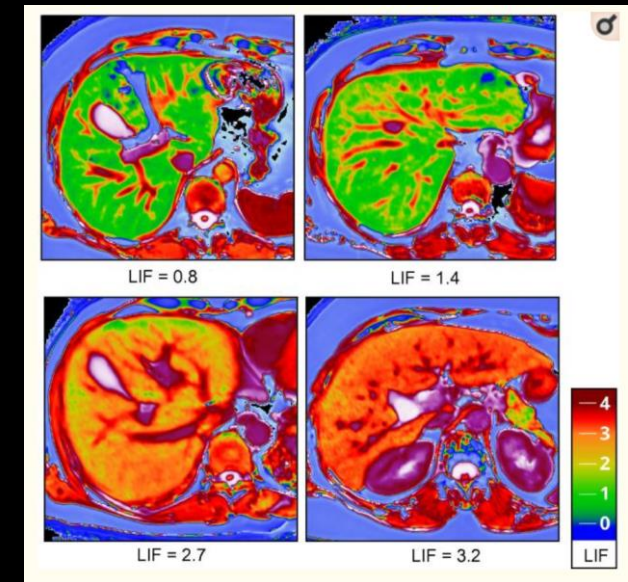




# Multi-parametric approach

- Liver *MultiScan* (LMS, Perspectum Diagnostics)

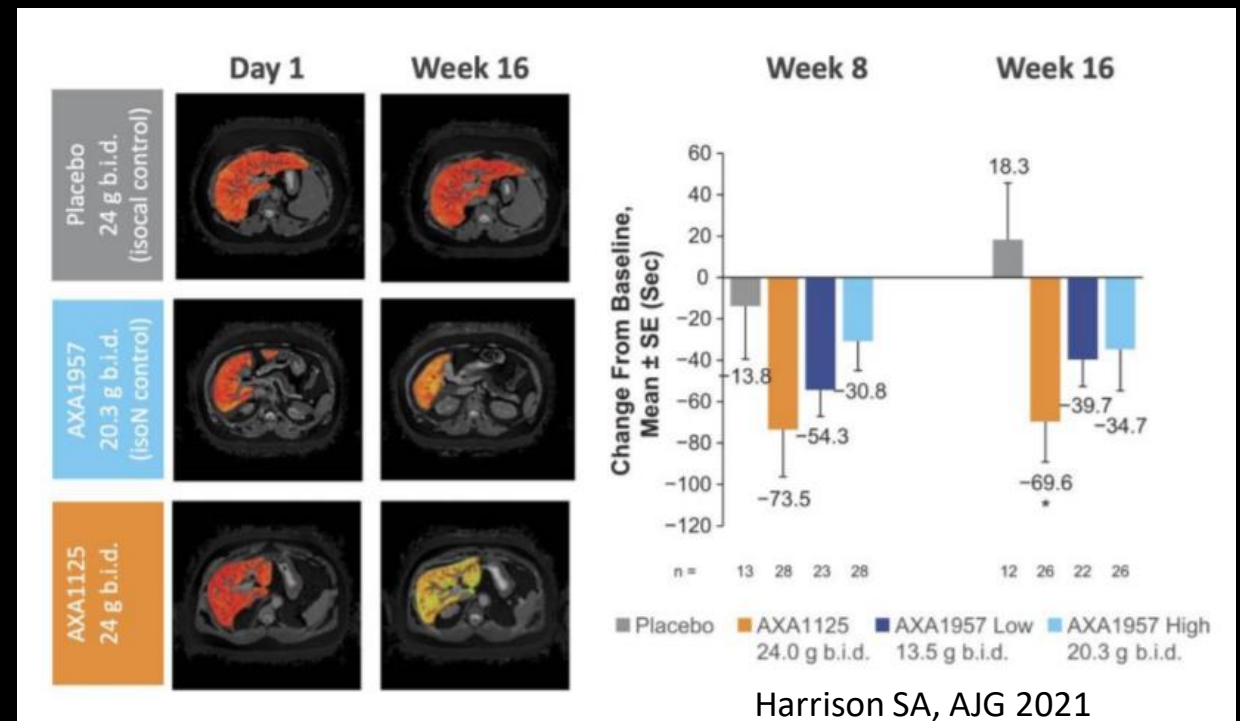
T1 map, T2\*, MRS or PDFF



Pavlidis M, J Hepatol 2016

## Emerging evidence (sample):

- Andersson A, Clin Gastro and Hepatol. 2021
- Beyer C, Plos One 2021
- Imajo K, World J Gastro. 2021
- Dennis A, Frontiers in Endo. 2021
- Pavlidis M, Liver Inter. 2017



Harrison SA, AJG 2021

# Summary

**MASLD**

**MASH**

**Cancer**

**GIB**

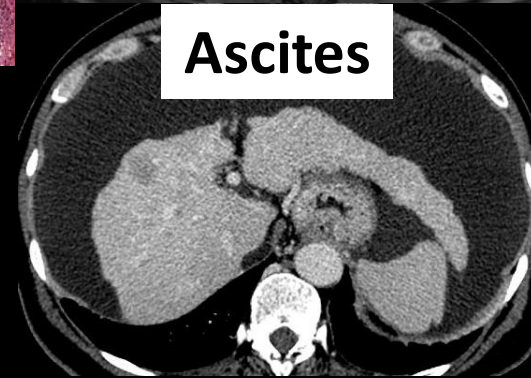
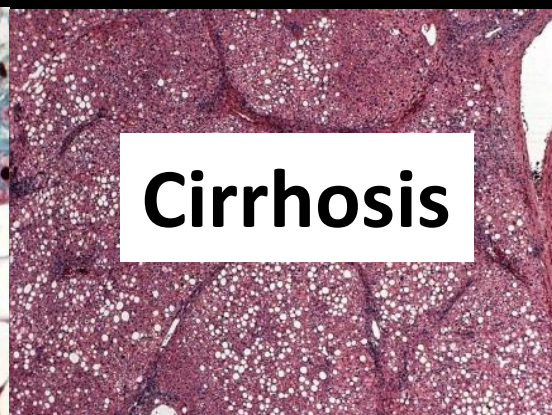
**Ascites**

**Fat**

**Inflammation**

**Fibrosis**

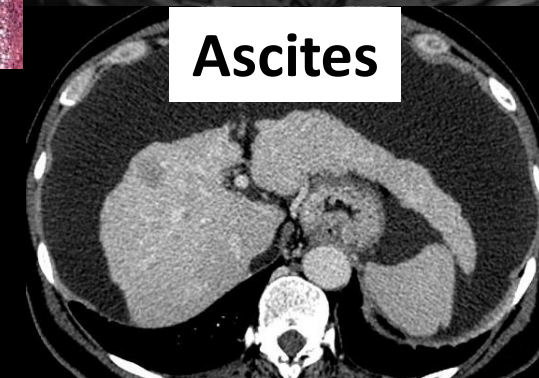
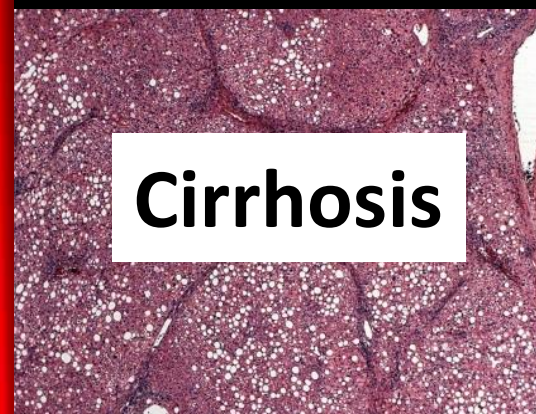
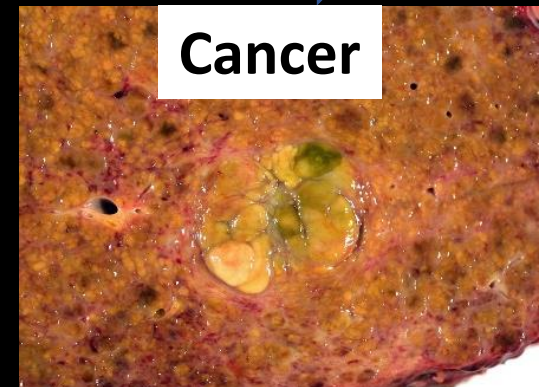
**Cirrhosis**



MASLD

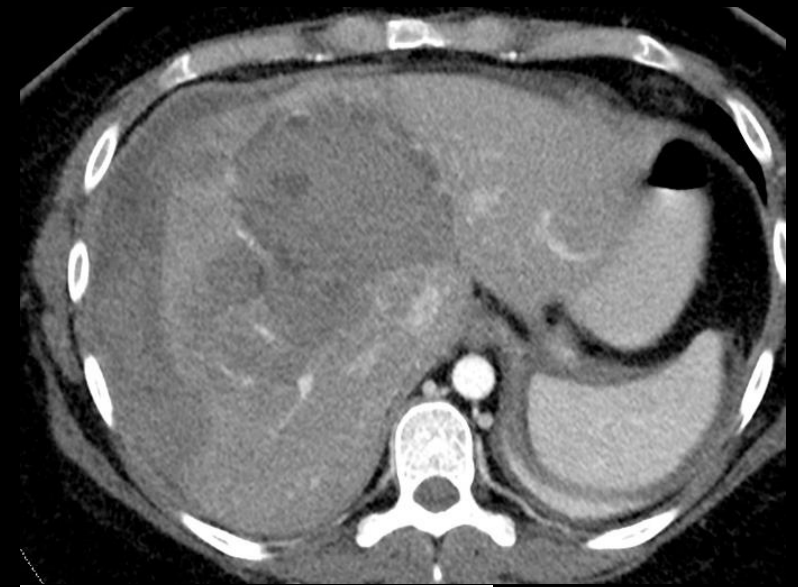
MASH

Silent!



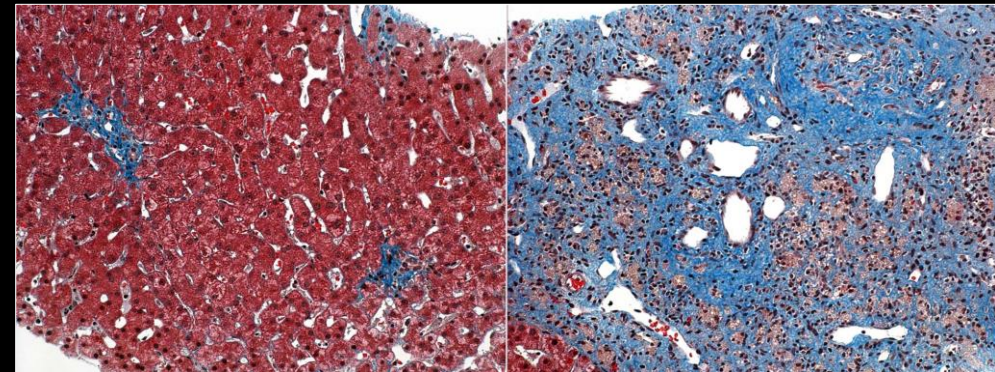
# MRI-PDFF is a QIB for liver fat

- Uses complex modeling- 'pure measure'
- Accurate and Precise
- Easy to perform, Single breath hold
- Validated across vendors and field strength



Noninvasive

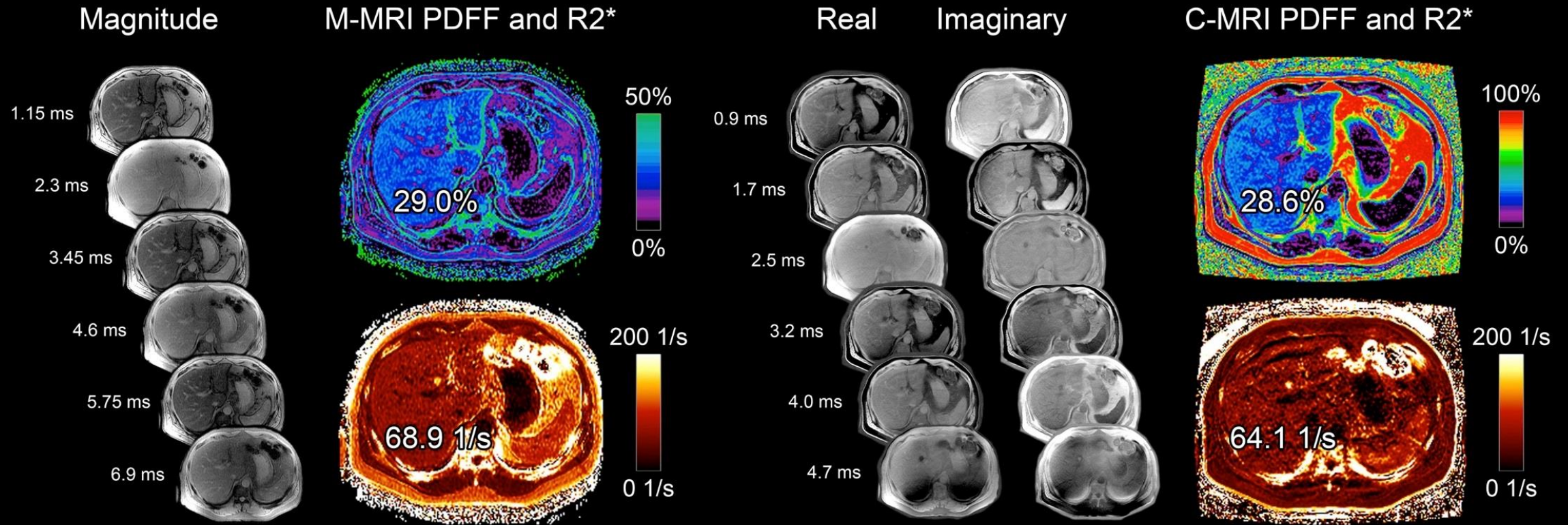
Minimal risk



Global

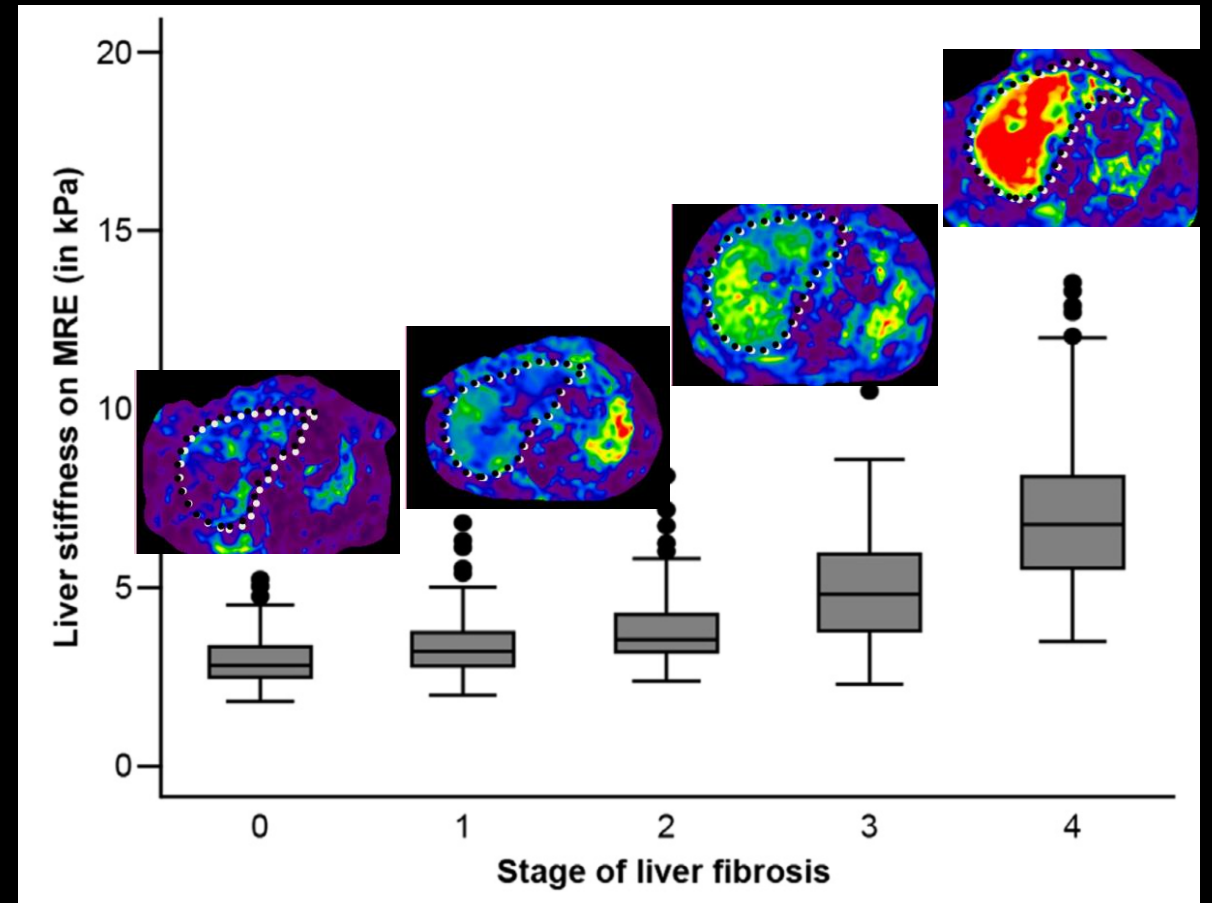
Same Patient-two biopsy cores

# $R_2^*$ Is a QIBM for Iron



# MRE is a QIB for liver fibrosis

- Non-invasive, minimal risk
- Standardized across systems
- Easy to perform
- Automated analysis now available
- Correlates with fibrosis/stages



# Conclusion

- MRI methods for fat, fibrosis, and iron are validated and in clinical use
- Inflammatory imaging biomarkers are still needed





# Thanks!

- [k1fowler@ucsd.edu](mailto:k1fowler@ucsd.edu)
- @chemshift1

- Stay tuned for quantitative imaging lexicon and guidance from LI-RADS

